EXHIBIT 5. SAR SYSTEM CONFIGURATION & TEST METHODOLOGY

5.1. MEASUREMENT SYSTEM SPECIFICATIONS

Positioning Equipment	Probe
Type : 3D Near Field Scanner Location Repeatability : 0.1 [mm] Speed 180 [^{o}/sec] AC motors	Sensor : E-Field Spatial Resolution : 1 [mm^3] Isotropic Response : ±0.25 [dB] Dynamic Range : 0.01 to 100 [W/Kg]
Computer	**Phantom**
Type : Pentium III 500MHz Memory : 256 MB RAM Operating System : Windows 2000 Pro Monitor : 19" SVGA	Tissue : Simulated Tissue with electrical characteristics similar to those of the human at normal body temperature. Left/Right Head: IEEE P1528 Compliant SAM manufactured by Aprel Body/Frontal Head: IEEE Flat Phantom 2 $_{[mm]}$ Base

5.2. TEST PROCEDURES

In the SAR measurement, the positioning of the probes must be performed with sufficient accuracy to obtain repeatable measurements in the presence of rapid spatial attenuation phenomena. The accurate positioning of the E-field probe is accomplished by using a high precision robot. The robot can be taught to position the probe sensor following a specific pattern of points. In a first sweep, the sensor is positioned as close as possible to the interface, with the sensor enclosure touching the inside of the phantom shell. The SAR is measured on a grid of points, which covers the curved surface of the phantom in an area larger than the size of the D.U.T. After the initial scan, a high-resolution volume gird is used to locate the absolute maximum measured energy point and to calculate the peak spatial-average SAR. At this location, attenuation versus depth scan will be accomplished by the measurement system in order to verify the peak spatial-average SAR measured.

5.3. PHANTOM

For Head mounted devices placed next to the ear, the phantom used in the evaluation of the RF exposure of the user of the wireless device is a IEEE P1528 compliant SAM phantom, shaped like a human head and filled with a mixture simulating the dielectric characteristics of the brain. A left sided head and a right sided head are evaluated to determine the worst case orientation for SAR. For body mounted and frontal held push-to-talk devices, a flat phantom of dimensions 70x42x20cm with a base plate thickness of 2mm is used.

5.4. SIMULATED TISSUE

Simulated Tissue: Suggested in a paper by George Hartsgrove and colleagues in University of Ottawa Ref.: Bioelectromagnetics 8:29-36 (1987)

Ingredient	Quantity
Water	40.4 %
Sugar	56.0 %
Salt	2.5 %
HEC	1.0 %
Bactericide	0.1 %

Table 5.4. Example of composition of simulated tissue

This simulated tissue is mainly composed of water, sugar and salt. At higher frequencies, in order to achieve the proper conductivity, the solution does not contain salt. Also, at these frequencies, D.I. water and alcohol is preferred.

Target Frequency	Head		Body	
(MHz)	ε_r	σ (S/m)	ε_r	σ (S/m)
150	52.3	0.76	61.9	0.80
300	45.3	0.87	58.2	0.92
450	43.5	0.87	56.7	0.94
835	41.5	0.90	55.2	0.97
900	41.5	0.97	55.0	1.05
915	41.5	0.98	55.0	1.06
1450	40.5	1.20	54.0	1.30
1610	40.3	1.29	53.8	1.40
1800 – 2000	40.0	1.40	53.3	1.52
2450	39.2	1.80	52.7	1.95
3000	38.5	2.40	52.0	2.73
5800	35.3	5.27	48.2	6.00

(ε_r = relative permittivity, σ = conductivity and ρ = 1000 Kg/m^{3*})

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[*] The actual mass density of the equivalent tissue vary based on the composition of the tissue from 990 Kg/m^3 to 1,300 Kg/m^3.

5.4.1. Preparation

The weight requirements is determined and measured carefully for all the components. A clean container is used where the ingredients will be mixed. A stirring paddle mounted to a drill press is used to stir the mixture. First the heat is applied to the DI water to approximately 40 ^{o}C to help the ingredients dissolve well and then the salt and the bactericide are added. It is stirred until all the ingredients are completely dissolved. It is continuously stirred slowly while adding the sugar. Rotation of stirring paddle at a high RPM is avoided to prevent air bubbles in the mixture. Later on, the HEC is added to maintain the solution homogeneous. Mixing time is approximately 2 hours.

5.5. MEASUREMENT OF ELECTRICAL CHARACTERISTICS OF SIMULATED TISSUE

1) Slotted Coaxial Waveguide
2) HP Dielectric Strength Probe System

5.5.1. Slotted Coaxial Waveguide

5.5.1.1. Equipment set-up

The test equipment consists of a slotted coaxial transmission line with a probe connected to a vector network analyzer, as shown in Figure 4.5.1.1. The log-magnitude and phase of S_{21} should be displayed simultaneously. Source power should be set to a level high enough to provide good signal-to-noise ratio. Periodically (annually or whenever the measuring scale along the line length is changed) a measurement is made on a reference liquid to validate the system. Since the measured quantities are magnitude and phase changes versus distance, the accuracy of the scale is very critical.

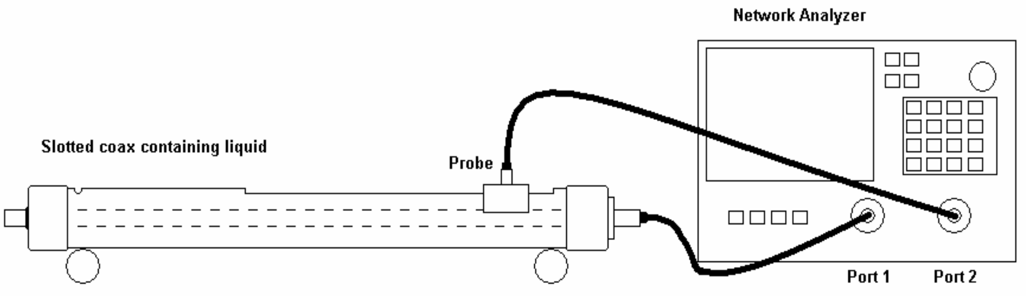


Figure 5.5.1.1. Slotted line set-up

The network analyzer injects a signal into one end of the slotted coaxial transmission line. The probe inserted through the slot into the tissue-equivalent material detects the RF amplitude and phase for each measurement position along the length of the line. A full two-port calibration of the network analyzer should be carried out prior to connecting the sample holder, and the following precautions should be observed:

a) Fill the slotted line carefully to avoid trapping air bubbles. This operation should be performed while the slotted line is horizontal.

b) The probe should be inserted into the slot at the end nearest to the input connector of the slotted line, ensuring that the tissue-equivalent liquid is flush with the inside surface of the line, and aligned with a well-defined position on the distance scale of the slotted line.

c) The probe should be inserted perpendicular to the slotted–line longitudinal axis until a stable and adequate amplitude response is achieved. Do not insert the probe too deeply into the coaxial line, because it can overly perturb the field distribution.

5.5.1.2. Measurement procedure.

a) Configure and calibrate the network analyzer.

b) Measure 10 to 20 log-magnitude and phase data points along the slotted line corresponding to about a 30 dB change in magnitude.

c) Plot S_{21} log-magnitude and phase vs. measurement distance.

d) Determine if the graphed points closely follow a straight-line approximation, based on the correlation coefficient or a similar statistical measure. The data should produce a good linear curve fit (expected correlation coefficient $r^2 > 0.99$ for lossy materials). If not, re-measure the liquid by increasing the sample points to extend the magnitude change from 30 to 40 dB. Note: for low loss materials, ensure that the slotted line is long enough to avoid reflections from the load-terminated end.

e) Calculate the conductivity and relative permittivity of the tissue-equivalent material using Equations (5.5.1.2.) derived from

$$\begin{aligned}
\overline{\alpha} &= \frac{m_m \ln(10)}{20} && \text{Np/cm} \\
\overline{\beta} &= \frac{m_p \pi}{180} && \text{rad/cm} \\
\varepsilon_r' &= \frac{(\overline{\beta})^2 - (\overline{\alpha})^2}{\omega^2 \mu_0 \varepsilon_0} && \\
\sigma &= \frac{2\overline{\alpha}\,\overline{\beta}}{\omega \varepsilon_0}\left(\frac{100\ \text{cm}}{\text{m}}\right) && \text{S/m}
\end{aligned} \qquad (5.5.1.2.)$$

where, m_m and m_p are the slopes of the least-squares linear fits of the log-magnitude and phase plots, respectively, and $\overline{\alpha}$ and $\overline{\beta}$ are the average attenuation and propagation coefficients along the line.

5.5.2. HP Dielectric Strength Probe System (open-ended coaxial transmission-line probe/sensor)

5.5.2.1. Equipment set-up

The equipment consists of a probe connected to one port of a vector network analyzer. The probe is an open-ended coaxial line, as shown in Figure B.2. Cylindrical coordinates (ρ, ϕ, z) are used where ρ is the radial distance from the axis, ϕ is the angular displacement around the axis, z is the displacement along the axis, a is the inner conductor radius, and b is the outer conductor inner radius.

The sample holder is a non-metallic container that is large compared with the size of the probe immersed in it. A probe with an outer diameter b of 2 to 4 mm is suitable for the measurement of tissue-equivalent materials in the 300 MHz to 3 GHz frequency range. This probe size is commensurate with sample volumes of 50 cc or higher. Larger probes of up to 7 mm outer diameter b may be used with larger sample volumes. A flange is typically included to better represent the infinite ground-plane assumption used in admittance calculations.

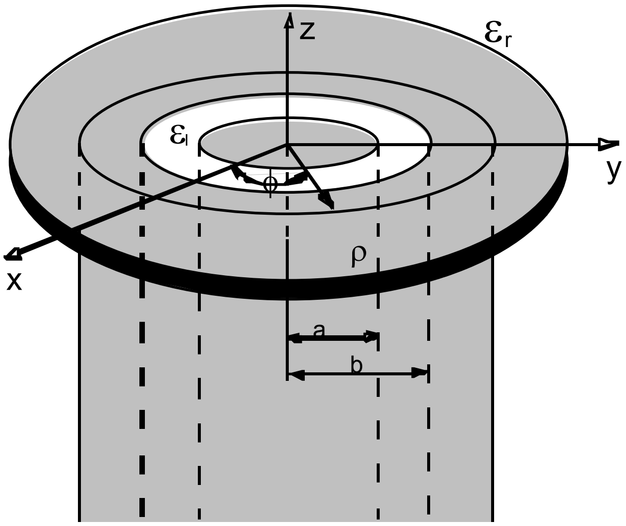


Figure 5.5.2.1. An open-ended coaxial probe with inner and outer radii *a* and *b*, respectively

The accuracy of the short-circuit measurement should be verified for each calibration at a number of frequencies. A short circuit can be achieved by gently pressing a piece of aluminum foil against the open end. For best electrical contact, the probe end should be flat and free of oxidation. Larger the sensors generally have better foil short-circuit repeatability. It is possible to obtain good contact with some commercial 4.6 mm probes using the metal-disk short-circuit supplied with the kit. For best repeatability, it may be necessary to press the disk by hand.

The network analyzer is configured to measure the magnitude and phase of the admittance. A one-port reflection calibration is performed at the plane of the probe by placing materials for which the reflection coefficient can be calculated in contact with the probe. Three standards are needed for the calibration, typically a short circuit, air, and de-ionized water at a well-defined temperature (other reference liquids such as methanol or ethanol may be used for calibration). The calibration is a key part of the measurement procedure, and it is therefore important to ensure that it has been performed correctly. It can be checked by re-measuring the short circuit to ensure that a reflection coefficient of $\Gamma = -1.0$ (linear units) is obtained consistently.

5.5.2.2. *Measurement procedure*

a) Configure and calibrate the network analyzer and probe system.

b) Place the sample in a non-metallic container and immerse the probe. A fixture or clamp is recommended to stabilize the probe, mounted such that the probe face is at an angle with respect to the liquid surface to minimize trapped air bubbles beneath the flange.

c) Measure the complex admittance with respect to the probe aperture.

d) Compute the complex relative permittivity $\varepsilon_r = \varepsilon_r' - j\sigma/\omega\varepsilon_0$.

5.6. SYSTEM CALIBRATION

The SAR measurement system has two main components:

a) the probe, which is connected to the inputs of
b) the instrumentation amplifier whose outputs are connected through the optical transmission line to
c) the computer.

The system is calibrated as one unit not as individual components. If any components is modified or replaced, the system must be re-calibrated.

The system calibration is performed by two steps:

1) determination of the sensitivity of the probe in the air by introducing it into the well-defined RF field, and
2) correlation of the measured E-field in the dielectric medium to the temperature rise in a dielectric medium.

5.6.1. Probe linearity

Detector diodes at the dipole feed-point are used to rectify the sensor voltage output. The rectified signal is transmitted through resistive (RF-transparent) lines to the sensor amplifier. At low field strength levels the output voltage is proportional to the square of the amplitude of the incident field; at higher signal levels, the output voltage is not linearly proportional to $|E|^2$, but becomes proportional to E. The compensation for diode compression is carried out for the each detector diode using the 3-rd order polynomial least-square fit algorithm before any further evaluation.

5.6.2. Free Space Calibration

Note: Equipment must be regularly calibrated.

- RF Signal Generator - frequency range to at least 6 GHz,
- RF Amplifier – if needed to generate the required power density in the test cell,
- Test Cell - TEM (Crawford) cell, waveguide, or other device capable of maintaining a uniform field,
- RF Power Meter - capable of measuring at least 5 Watts (current calibration is mandatory!) if possible traceable to the National Institute of Standards and Technology (NIST).
- E-Field Probe (under calibration)
- Probe Support Fixture
- Instrumentation Amplifier
- Transmission Line
- Computer Program with the Automated Calibration System Program

5.6.2.1. Method

Due to impedance variations in the diodes and the transmission line, and slight differences in gain among the channels of the instrumentation amplifier, a normalization method had been designed. The calibration method actually used is to determine the factors necessary adjust each channel of the system so it's indicated output can then be equated to the well-defined RF field. These factors are referred to as "Amplifier Settings".

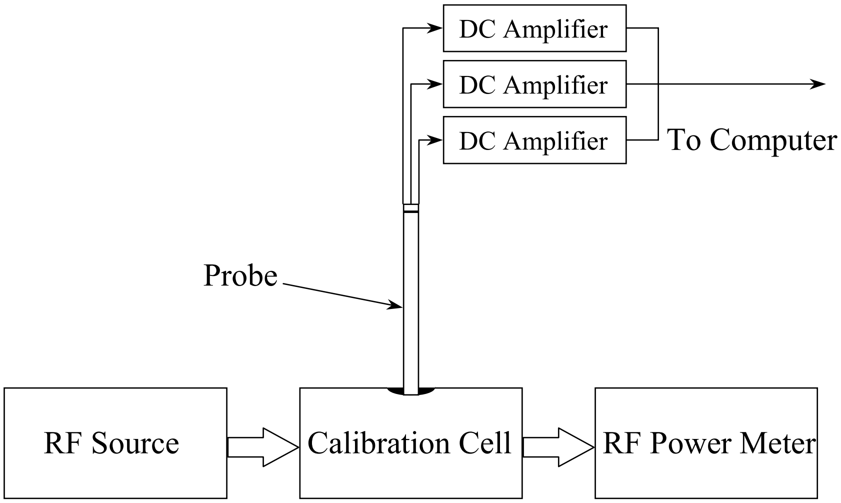


Figure 5.6.2.1. Free Space Calibration Setup for Amplifier Setting

5.6.2.2. Measurement procedure

Free Space Calibration of E-field probes can be performed using a TEM cell manufactured by IFI (Instrumentation for Industry, Farmingdale, NY 11735) with operating frequency at or below 1 GHz. Above 1 GHz, waveguides are used to calibrate the probes in free space.

- Connect the equipments as shown in Figure 5.6.2.1;
- Adjust the RF generator output so that the power density at the calibration point inside the TEM cell is well-defined. (For the IFI model CC-110 cell, the uniform power density of 1.0 [mW/cm^2] requires the power level of 271.0 [mW]);
- Mount the probe of the system to calibrate in the support fixture. Insert the probe through the aperture of the TEM cell. The probe handle should be at the geometric center of the aperture, i.e. midway between the septum and the upper surface, and orthogonal to the side of the cell. The sensing portion of the probe should be located at a point halfway across the depth of the cell (volumetric center).

- Once the prescribed position is obtained, it must be maintained during the rest of the measurement. The only movement of the probe allowed is rotation on its axis to position the dipole in the plane of the E-field and, for channel 3 only, parallel to the vertical uniform field (max./min. output).
- Verify that the RF power level remains constant throughout the measurement. While the probe is being rotated through 360 degrees, software indicators will show the maximum measured on each channel.

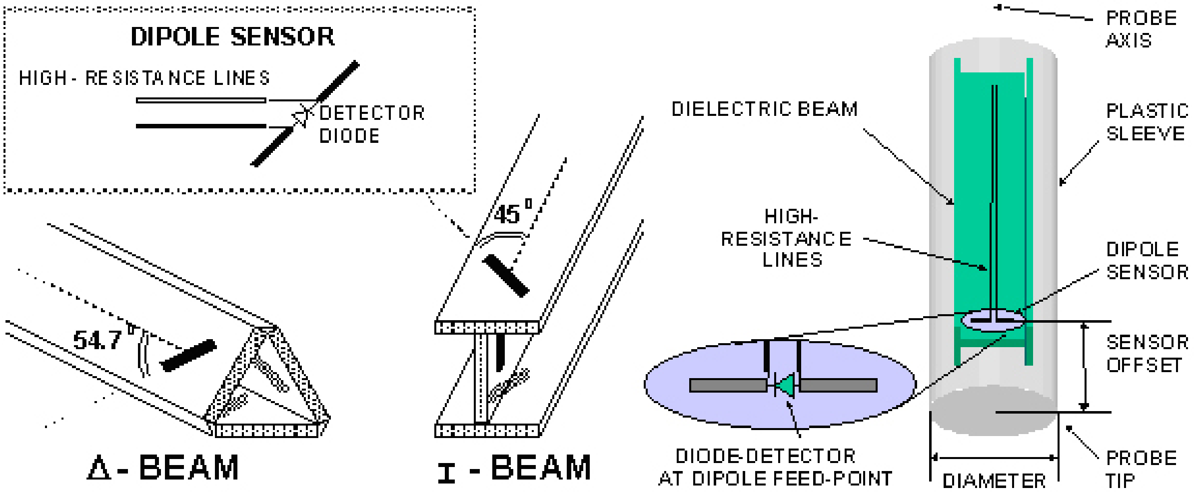


Figure 5.6.2.2. E-field probe construction

5.6.2.3. *Definition of Amplifier Settings*

The initial sequence of probe calibrations steps performed with SAR determinations produces the factors used in scaling probe output voltage to RF power density. For historical reasons all probes factors are compared to a factor 10.8 [mV] per [mW/cm^2] that was typical of a prototype probe, but is in fact an arbitrary number used as an intermediately constant. The factor of 10.8 [mV/(mW/cm^2)] is known as the sensor factor to the uniform power density (η_{pd}), but does not change. Also we can derive 10.8/3,770 [mV/(V/m)^2] of the sensor factor to the $|E|^2$ (η_{E2}), providing 377 [Ω] as free space impedance.

$$\eta_{Pd} = 10.8[mV/(mW/cm^2)] \equiv \eta_{E2} = \frac{10.8}{3770}[mV/(V/m)^2]$$

$$Pd[mW/cm^2] = \frac{PO_{tot}}{\eta_{Pd}},\ |E|^2[(V/m)^2] = \frac{PO_{tot}}{\eta_{E2}} \text{ and } SAR = \frac{\sigma \times \frac{PO_{tot}}{\eta_{E2}}}{\rho}$$

To calibrate a probe, each channel is assigned an amplifier setting. This factor is obtained from the maximum probe output voltage measured during probe calibration. This probe output voltage is corrected for any DC offset of the instrumentation amplifier, usually a very small amount.

During calibration, the sensitivity for the E-field tangential to the dipole axis caused by the geometry of the probe construction is carefully considered to obtain the correct amplifier setting for each channel. Thus, the amplifier settings for each channel are as follows:

$$AS_i = \frac{\eta_{Pd}}{V_{\max_i} - DC_i} \times \cos^2(\varphi - \theta_i) \times Pd$$

Where,

AS_i	Amplifier Setting for channel i
η_{pd}	Sensor Factor to the uniform power density, an arbitrary value 10.8 [mV/(mW/cm^2)]
V_{maxi}	Maximum probe raw output recorded for channel i by rotation about the probe axis with the probe in a test cell
DC_i	Ambient DC offset of channel i (the voltage output of the transmission line with the instrumentation amplifier on and RF power off, recorded at the beginning of the probe calibration)
φ	Smaller angle between the probe axis and the direction of the E-field (90° providing the probe axis is parallel to the plane of the septum inside TEM cell)
θ_i	Smaller angle between the probe axis and the dipole sensor axis of the channel i ($\theta_1 = \theta_2 = 45°$, $\theta_3 = 90°$ for I-beam probe, and $\theta_1 = \theta_2 = \theta_3 = 54.7°$ for triangular-beam probe)
Pd	Well-defined power density [mW/cm^2] at the calibration point in a test cell

5.6.3. Thermal Transfer Calibration

5.6.3.1. Measurement procedure

An RF transparent thermistor-based temperature probe and a isotropic E-field probe are placed side-by-side in a planar phantom while both are exposed to RF energy from a half wave dipole antenna located below the phantom The E-field probe and amplifiers were previously calibrated.

First, the location of the maximum E-field close to the phantom's bottom is determined as a function of power into the dipole

Then, the E-field probe is moved sideways so that the temperature probe, while affixed to the E-field probe is placed at the previous location of the E-field probe.

Finally, temperature changes for a certain amount of time (generally 10 to 30 seconds) exposures at the same RF power levels used for the E-field are recorded. Care is taken to allow cooling down to the original temperature and temperature stabilization between tests.

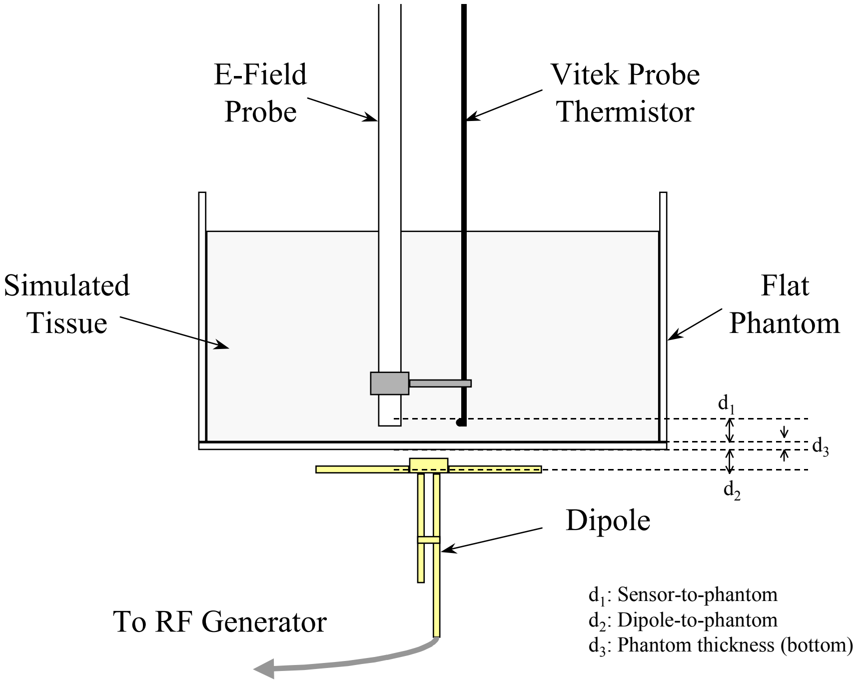


Figure 5.6.3.1. Flat Phantom, Thermistor and E-Field Probe

The following simple equation relates SAR to the initial temperature slope:

$$SAR_t = \frac{c \cdot \Delta T}{\Delta t} \qquad \text{(Eq. 1)}$$

In (Eq.1) Δt is the exposure time [sec], c is the specific heat capacity of the simulated tissue [J/Kg/ ^{o}C] and ΔT is the temperature increase [^{o}C] due to the RF exposure. SAR is proportional to ΔT/Δt, the initial rate of tissue heating, before thermal diffusion takes place.

From (Eq.1) it is possible to quantify the electric field in the simulated tissue by equating the thermally-derived SAR to the E-field:

$$SAR = \frac{|E|^2 \cdot \sigma}{\rho} \qquad \text{(Eq. 2)}$$

where σ is the simulated tissue conductivity [S/m] andρ its mass density [Kg/m^3]; The actual mass density of the simulated tissue is required during the thermal transfer calibration, while mass density of 1,000 [Kg/m^3] is conventionally chosen during the SAR measurements.

5.6.3.2. Determination of Conversion Factor (γ) in the simulated tissue

The sensitivity of the probe in the dielectric media compared to its sensitivity in the air, is different. Conversion Factor (γ) is defined to determine the degree of the enhancement of sensitivity in the different dielectric media and relate it to its sensitivity in the air.

$$PO_{tot\_tissue} \equiv PO_{tot\_air} \times \gamma$$

Thus,

$$\left|E_{tissue}\right|^2 = \frac{PO_{tot\_tissue}}{\eta_{E2}} \times \frac{1}{\gamma} \quad \text{,and} \quad SAR_{tissue} = \frac{\sigma \times \dfrac{PO_{tot\_tissue}}{\eta_{E2}} \times \dfrac{1}{\gamma}}{\rho}$$

where,

$\lvert E_{tissue}\rvert^2$	RMS E-field level $[(V/m)^2]$ induced within the exposed tissue
PO_{tot_tissue}	Probe voltage output measured in the simulated tissue [mV]
PO_{tot_air}	Probe voltage output measured in the air ($Z_{air} = 377[\Omega]$) [mV]
η_{E2}	Sensor Factor to the $\lvert E\rvert^2$, an arbitrary value 10.8/3,770 $[mV/(V/m)^2]$
γ	Conversion factor; ratio of sensor response in air to response in the dielectric media

The conversion factor (γ) can be used to scale the E-field in terms of the thermally-derived SAR. It is the quotient of SAR_t, the SAR determined from temperature measurements in the flat phantom, and PO_{tot_tissue}, the E-field prove output voltage obtained at the same location in the phantom

$$SAR_t = SAR_{tissue}$$

$$\frac{c \cdot \Delta T}{\Delta t} = \frac{\sigma_{@cal} \times \left|E_{tissue}\right|^2}{\rho}$$

$$= \frac{\sigma_{@cal} \times \dfrac{PO_{tot\_tissue}}{\eta_{E2}} \times \dfrac{1}{\gamma}}{\rho}$$

Thus,

$$\gamma = \frac{\sigma_{@cal}}{\eta_{E2} \times \rho} \times \frac{PO_{tot\_tissue}}{SAR_t} = \frac{\sigma_{@cal} \times 3{,}770}{10.8 \times c \times \rho} \times \frac{PO_{tot\_tissue}}{\Delta T / \Delta t} \qquad \text{(Eq. 3)}$$

where,

γ	Conversion factor; ratio of sensor response in air to response in the dielectric media
SAR_t	Thermally-derived SAR [W/Kg] (Eq. 1)
$\lvert E_{tissue}\rvert^2$	RMS E-field level $[(V/m)^2]$ induced within the exposed tissue
PO_{tot_tissue}	Probe voltage output measured in the simulated tissue [mV]
η_{E2}	Sensor Factor to the $\lvert E\rvert^2$, an intermediately constant, 10.8/3,770 $[mV/(V/m)^2]$
c	Specific heat capacity of the simulated tissue [J/Kg/ °C]
$\sigma_{@cal}$	Conductivity of the simulated tissue during the calibration procedure [S/m]
ρ	Actual mass density of the simulated tissue $[Kg/m^3]$
$\Delta T/\Delta t$	Initial rate of tissue heating, before thermal diffusion takes place [°C /sec]

The temperature E-field correlation is illustrated below (for simulated brain tissue) for an example in which the thermal quantities were,

RF power input = 0.5 [W]
$\Delta T = 0.0163$ [°C] (from thermistor-base temperature probe)
$\sigma_{@cal} = 0.97$ [S/m]
$\rho = 1,200$ $[Kg/m^3]$
c = 2,700 [J/Kg/°C]
$\Delta t = 30$ [sec]

The resulting SAR_t was (Eq. 1)

$$SAR_t = \frac{2,700 \times 0.0163}{30} = 1.467 \text{ [W/Kg]}$$

In this case the output of the E-field probe when at the same position as the thermistor probe was

$$PO_{tot\_tissue} = 28.5 \text{ [mV]}$$

The calculation of conversion factor (γ) from (Eq. 3) follows:

$$\gamma = \frac{0.97}{\frac{10.8}{3,770} \times 1,200} \times \frac{28.5}{1.467} = 5.482$$

5.6.4. Data Acquisition Methodology

5.6.4.1. E-Field Measurement

The probe calibration must be current before starting measurements. Instrumentation amplifier batteries must be charged. This can be monitored by observing DC offset voltages. A daily log of the DC offset voltages should be kept for this purpose.

Measurements in the phantom are automatically calculated for each location by summation of the three dipole outputs. Because each dipole produces an output voltage proportional to the square of the electric field component along the dipole, the sum of dipole voltages represents the RMS values for the total electric field. Thus, taking into consideration the amplifier settings and the DC offset voltages, the total electric field strength at a measurement location is as follows. See Appendix C. PO_{tot} is labeled by the software as measure of values (voltages). The SAR for calculations that are derived from the measure of values are discussed below.

At each measurement point, the program records the output of the three channels:

$$PO_1 = (V_1 - DC_1) \times AS_1 \equiv |E_1|^2 \times \eta_{E2}$$
$$PO_2 = (V_2 - DC_2) \times AS_2 \equiv |E_2|^2 \times \eta_{E2}$$
$$PO_3 = (V_3 - DC_3) \times AS_3 \equiv |E_3|^2 \times \eta_{E2}$$

$$\begin{aligned} PO_{tot} &\equiv |E|^2 \times \eta_{E2} = \left(|E_1|^2 + |E_2|^2 + |E_3|^2\right) \times \eta_{E2} = |E_1|^2 \times \eta_{E2} + |E_2|^2 \times \eta_{E2} + |E_3|^2 \times \eta_{E2} \\ &\equiv PO_1 + PO_2 + PO_3 \end{aligned}$$

Where,

V_i	Actual raw reading of channel i at a measurement point
DC_i	Ambient DC offset of channel i at a measurement point
AS_i	Amplifier setting of channel i
η_{E2}	Sensor Factor to the $|E|^2$, an arbitrary value 10.8/3,770 [mV/(V/m)^2]
PO_i	Probe output of channel i at a measurement point [mV]
PO_{tot}	Total probe output at a measurement point [mV]

5.6.4.2. *Sensitivity(ζ) of probe in the simulated tissue*

The sensitivy(ζ) of the probe in the simulated tissue is rendered in terms of Sensor Enhancement Factor in the simulated tissue.

$$\zeta = \frac{\sigma_{@meas}}{\eta_{E2} \times \rho \times \gamma} = \frac{\sigma_{@meas}}{\frac{10.8}{3,770} \times 1,000 \times \gamma} = \frac{3,770 \times \sigma_{@meas}}{10,800 \times \gamma} \qquad \text{(Eq. 5)}$$

Where,

ζ	Sensitivity of the probe in the simulated tissue [W/Kg/mV]
γ	Conversion factor; ratio of sensor response in air to response in the dielectric media
η_{E2}	Sensor Factor to the $|E|^2$, an arbitrary value 10.8/3,770 [mV/(V/m)^2]
$\sigma_{@meas}$	Conductivity of the simulated tissue during the measurement [S/m]
ρ	Mass density of the simulated tissue [Kg/m^3]; 1,000 [Kg/m3] is conventionally chosen.

Therefore, SAR can be yielded from

$$SAR = \zeta \times PO_{tot\_tissue} \qquad \text{(Eq. 6)}$$

Where,

ζ	Sensitivity of the probe in the simulated tissue [W/Kg/mV]
PO_{tot_tissue}	Probe voltage output measured in the simulated tissue [mV]

To continue the example illustrated above,

$\sigma_{@meas}$ = 0.99 [S/m]
PO_{tot_tissue} = 11.5 [mV]

$$\zeta = \frac{3{,}770 \times \sigma_{@meas}}{10{,}800 \times \eta} = \frac{3{,}770 \times 0.99}{10{,}800 \times 5.482} = 0.063 \text{ [W/Kg/mV]}$$

$$SAR = \zeta \times PO_{tot\_tissue} = 0.063 \times 11.5 = 0.725 \text{ [W/Kg]}$$

5.6.4.3. SAR Measurement

The goal of the measurement process is to scan the phantom over a selected area in order to find the region of highest levels of RF energy and then to obtain a single value for the peak spatial-average of SAR over a volume that would contain one gram (in the shape of a cube) of biological tissue. The test procedure, of course, measures SAR in the simulated tissue.

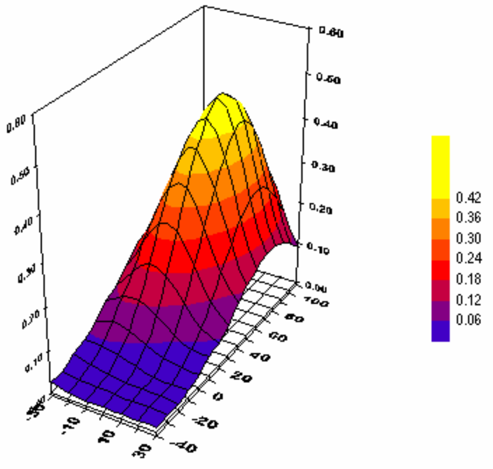


Figure 5.6.4.3.a. Area scan

The software request the user to move the probe to locations at two extreme corners of a rectangle that encloses the area to be scanned. An arbitrary origin and the spatial resolution for the scan are also specified. Under program control, the scan is performed automatically by the robot-guided probe.

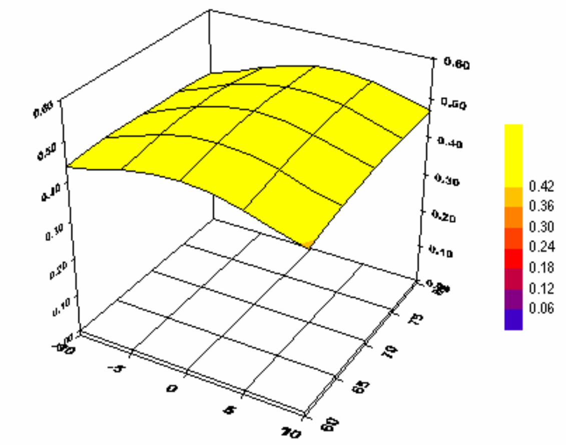


Figure 5.6.4.3.b. Zoom Scan

The fine resolution volume scan region is centered at the peak SAR locations determined by the interpolated (cubic spline) data from the area scan measurements. The number of measurement point required in a zoom scan is defined to provide an accurate one-gram averaged SAR in terms of both the number of points ($PT_X \times PT_Y \times PT_Z$) and the size ($SZ_X[mm] \times SZ_Y[mm] \times SZ_Z[mm]$) of the cubic. For one-gram SAR, ($5 \times 5 \times 7$) and ($32[mm] \times 32[mm] \times 30[mm]$) is preferred to select below 1 GHz. The zoom scan region extends in each direction for at least 1.5 times the linear dimensions of 1- or 10-gram cube of tissue from each peak. The zoom scan spatial resolution is interpolated down to SAR values on a 1mm grid by using the tri-linear interpolation algorithm.

The peak field values near the surface of a homogeneous phantom are usually not measurable because the sensors in a field probe are located at 2-4 mm behind the tip of the probe and the measurement point is defined at the geometric center of the sensors where the calibration is defined. These SAR values are computed by extrapolating the closest measured points to the surface of the phantom to determine the highest one-gram averaged SAR. The extrapolation coefficients are determined with a multi-order curve-fitting algorithm. Generally the 4-th order polynomial least-square fit is sufficient to extrapolate to the surface if the number of the valid measurements, that are non-zero, along the probe axis is greater than 4.

The interpolated and extrapolated SAR values from the zoom scan measurements are integrated in the shape of 1- or 10-gram cube then traversed to determine the highest peak spatial-average SAR in the zoom scan region.

This peak spatial-averaged SAR is reported as SAR [W/kg] for compliance.

5.6.4.4. Data Extrapolation and boundary effect

The distance from the center of the sensor (diode) to the end of the protective tube is called the 'probe offset' or 'sensor offset'. To compensate we use a multi-order polynomial least-square curve fitting to obtain the peak surface value from the voltages measured at the distance from the inner surface of the phantom. The field is measured as close as possible to the phantom's surface and every pre-defined separation distance (1 [mm] to 5 [mm]) along the probe axis (z) for a distance of at least 50 mm until they are not measurable. The appropriate curve is obtained from all the points measured and used to define an exponential decay of the energy density versus depth.

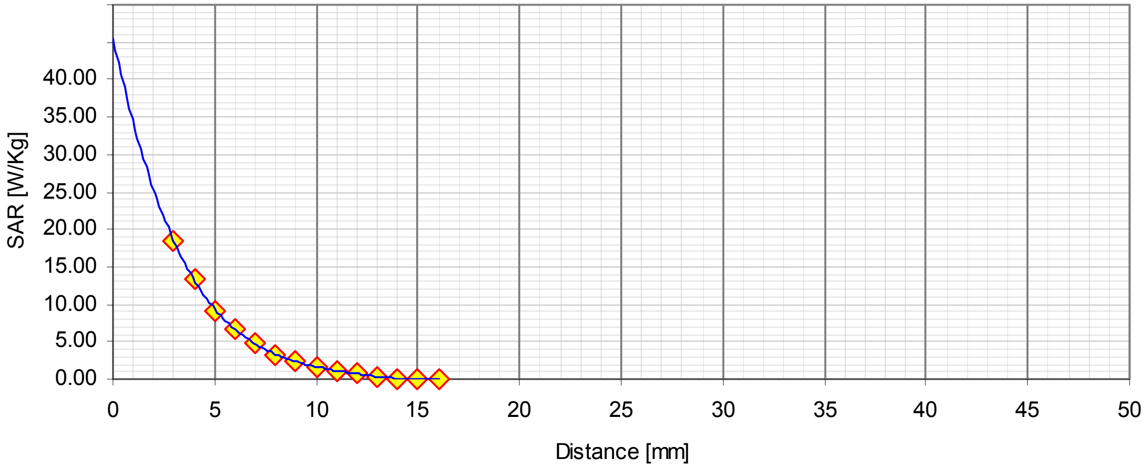


Figure 5.6.4.4. Exponential decay of the energy density versus depth

Boundary effects arise when the tip of an electric field probe approaches the interface between two dielectric media. Under these conditions, the external field is strongly perturbed by the superposition of a scattered field from the probe. The effect of the boundary on the peak spatial-average SAR values strongly depends on the probe dimensions, especially the diameter of the tip of the probe. It is known that the error due to boundary effects is very small if the distance between the probe tip and the surface is greater than half the probe diameter. Therefore the first one or two measurements at the vicinity to the phantom surface are excluded for evaluating the exponential decay curve in order to compensate for the boundary effect.

5.6.5. Determining the Heat Capacity of Simulated Tissue

5.6.5.1. Instruments and Materials

- Calibrated differential thermometer (Vitek or BAT-8 or equivalent)
- Two identical 500 ml containers

- A thermally insulated vessel (thick styrofoam, with a form fitting hole for one container)
- Hot and cold tap water
- Solution under test
- Hot plate
- Temperature vs. time (chart recorder, or data loger)

5.6.5.2. *Method*

Heat can be propagated by conduction, convection and radiation. In the case of liquids heated from below, gravity convection is the main and predominant heating mechanism of the fluid mass.

Obtain two containers that can be rapidly heated (e.g. glass or suitable plastic). Fill one container with 250 ml of water, the other with the same mass of simulated tissue. The initial temperature of the water should be the same as that of the simulated tissue ($\pm$1°C). Since we are dealing with heating by electromagnetic sources at ambient temperature, it is essential that we eliminate the chance of any direct infrared heating of the temperature sensor. To ensure this, position the tip of the sensor 2 mm from the bottom of the center of the container. Turn on the heat source and wait at least 5 minutes for its temperature to stabilize. Record the initial temperature of the water. Place the container of water 5 mm above the center of the hot plate and monitor the temperature increase.

After 30 seconds of heating, the water temperature should have increased by at least 5 °C. Record the time and temperature. Remove the container from the heat source and place it in the thermally insulated vessel. Stir the liquid thoroughly and record the steady state temperature 1-2 minutes after stirring.

Repeat the above procedure using the container of simulated tissue. Ensure that the container is placed on the same area of the hot plate, is heated for the identical length of time, and the steady state temperature is recorded after the identical time interval.

Since the heat capacity of water is C_w = 1,000 [cal/Kg/°C] or 4,189 [J/Kg/°C] with excellent approximation (~1%) in the temperature range of interest, the heat capacity (C_s) of the solution is given by:

$$C_s = C_w \cdot \frac{\Delta T_w}{\Delta T_s}$$

where ΔT_w is the temperature increase of water and ΔT_s the temperature increase of the solution. The ration of the values, $\Delta T_w / \Delta T_s$, should be the same (within the sensitivity of the thermometer) at the end of the heating and stirring. This ensures that the liquids have been uniformly heated.

5.6.5.3. *Rationale*

$$C \cdot \Delta T = Heat\_Flow \cdot Time = Total\_Heating\_Energy$$

If the heat flow, sample mass, and absorption (heat transfer) are the same for both liquids, then:

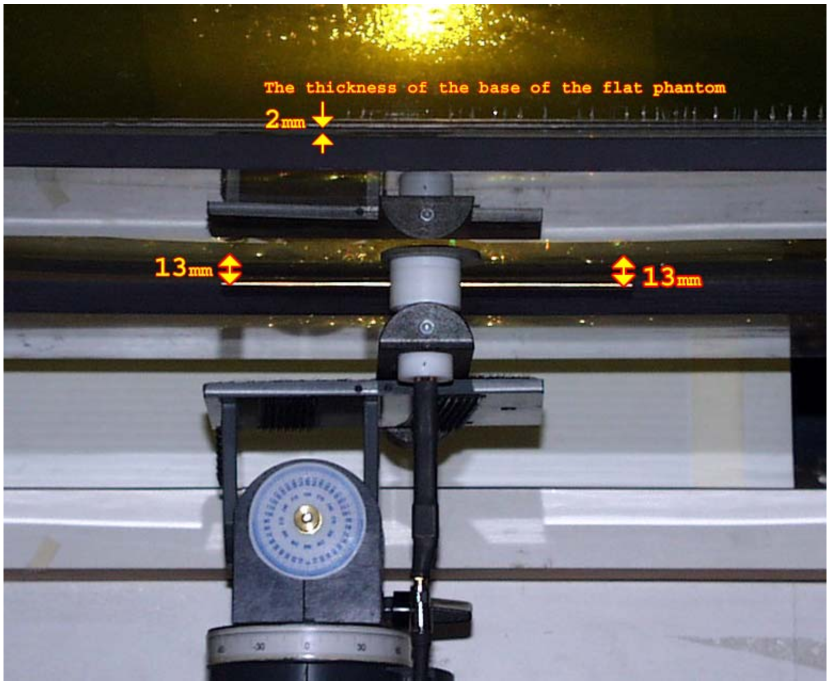
$$C_w \cdot \Delta T_w = C_s \cdot \Delta T_s$$

The heat flow and total heating are kept constant by using the same source for the same amount of time. If the heat transfer mechanisms for the two liquids are about the same, with insignificant differences in convective and conductive characteristics, then any differences in temperature increase are a direct measure of the specific heat capacity, C.

5.7. SAR MEASUREMENT SYSTEM VERIFICATION

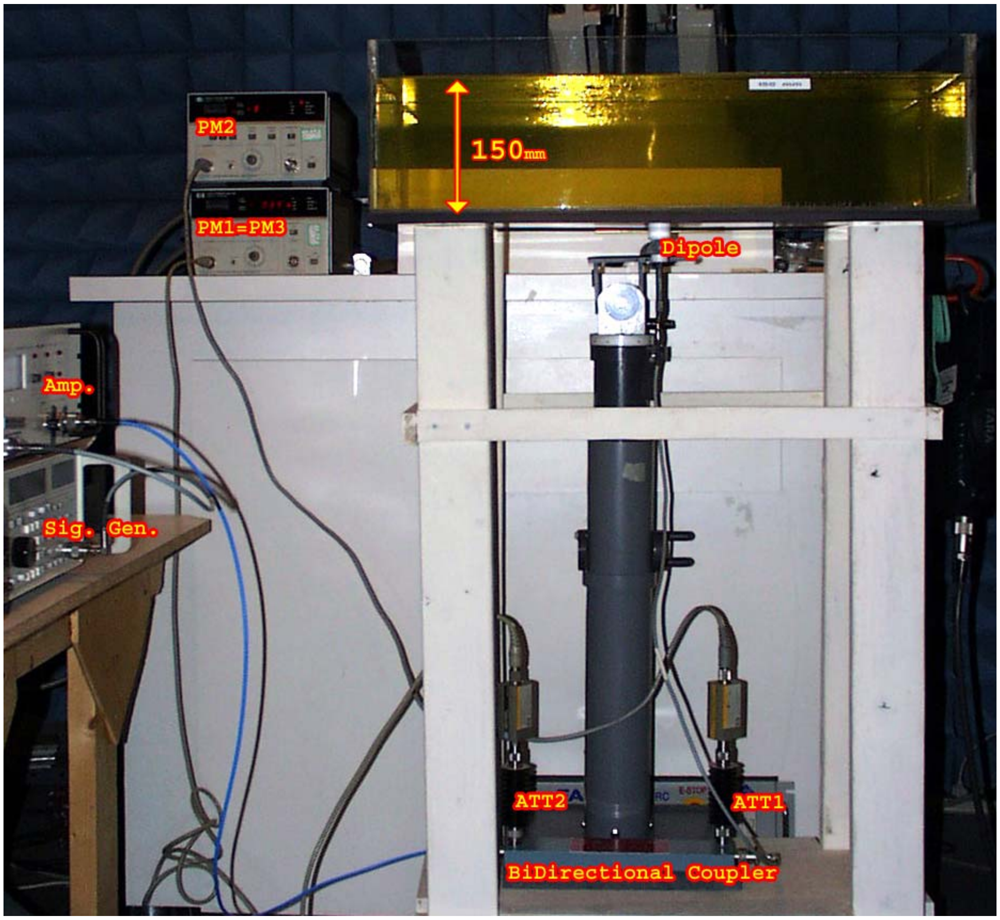
5.7.1. Standard Source

A half-wave dipole is positioned below the bottom of the phantom and centered with its axis parallel to the longest side of the phantom. The distance between the liquid filled phantom bottom surface and the center of the dipole axis, *s*, is chosen as specified IEEE 1528 at the specific test frequency (i.e. 15 mm at 835 MHz). A low loss and low dielectric constant spacer is used to establish the correct distance between the top surface of the dipole and the bottom surface of the phantom.



5.7.2. Standard Source Input Power Measurement

The system validation is performed as shown below or in Figure 7.1 in IEEE 1528.



First the power meter PM1 (including attenuator Att1) is connected to the cable to measure the forward power at the location of the dipole connector (X). The signal generator is adjusted for the desired forward power at the dipole connector (taking into account the attenuation of Att1) as read by power meter PM2. After connecting the cable to the dipole, the signal generator is readjusted for the same reading at power meter PM2. If the signal generator does not allow adjustment in 0.01dB steps, the remaining difference at PM2 must be taken into consideration. PM3 records the reflected power from the dipole to ensure that the value is not changed from the previous value. The reflected power was verified to be at least 20dB below the forward power.

5.7.3. System Validation Procedure

A complete 1g-averaged SAR measurement is performed. The measured 1g-averaged SAR value is normalized to a forward power of 1W to a half-wave dipole and compared with the reference SAR value for the reference dipole and flat phantom shown in columns 2 and 3 of Table 7.1 in IEEE 1528.

5.8. POWER MEASUREMENT

Whenever possible, a conducted power measurement is performed. To accomplish this, we utilize a fully charged battery, a calibrated power meter and a cable adapter provided by the manufacturer. The data of the cable and related circuit losses are also provided by the manufacturer. The power measurement is then performed across the operational band and the channel with the highest output power is recorded.

Power measurement is performed before and after the SAR to verify if the battery was delivering full power at the time of testing. A difference in output power would determine a need for battery replacement and to repeat the SAR test.

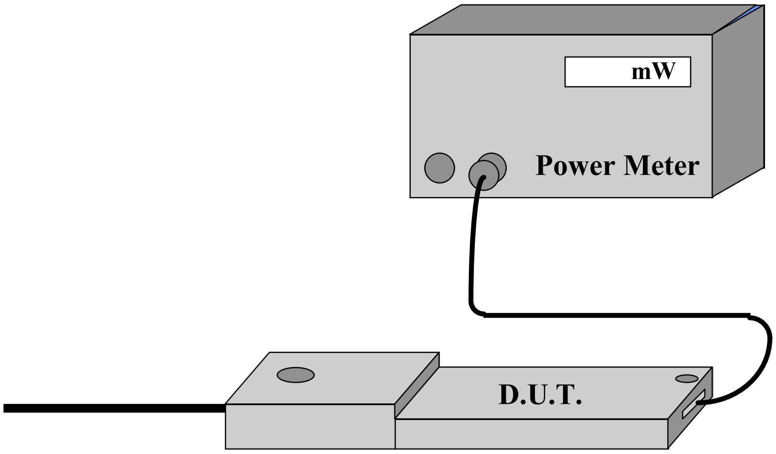


Figure 5.8. Measured Power + Cable and Switching Mechanism Loss

5.9. POSITIONING OF D.U.T.

The clear SAM phantom shell have been previously marked with a highly visible grid with a defined centre line, so it can easily be seen through the liquid simulated tissue. In the case of testing a cellular phone, this line is connecting the ear channel with the corner of the lips. The D.U.T. is then placed by centering the speaker with the ear channel and the center of the radio width with the corner of the mouth.

For HAND HELD devices (push-to-talk), or any other type of wireless transmitters postioned in front of the face, the D.U.T. will be positioned 2.5cm distance from a flat phantom to simulate the frontal facial position in use. All body-worn operating configurations are tested using a flat phantom. The length and width of the phantom is at least twice the corresponding dimensions of the test device, including its antenna.

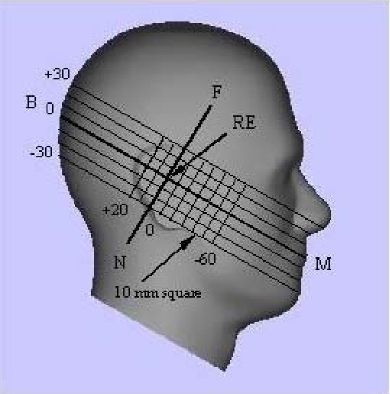


Figure 5.9.a. Side view of the phantom showing relevant marking

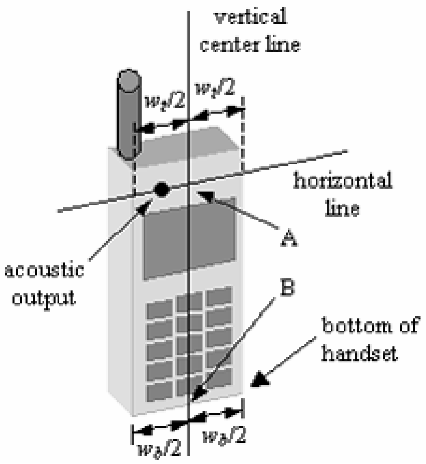


Figure 5.9.b. Handset vertical and horizontal reference lines – fixed case

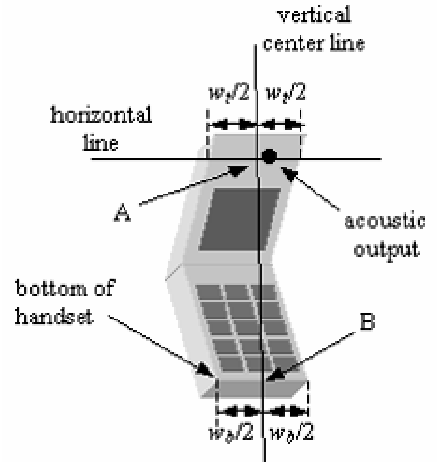


Figure 5.9.c. Handset vertical and horizontal reference lines – “clam-shell”

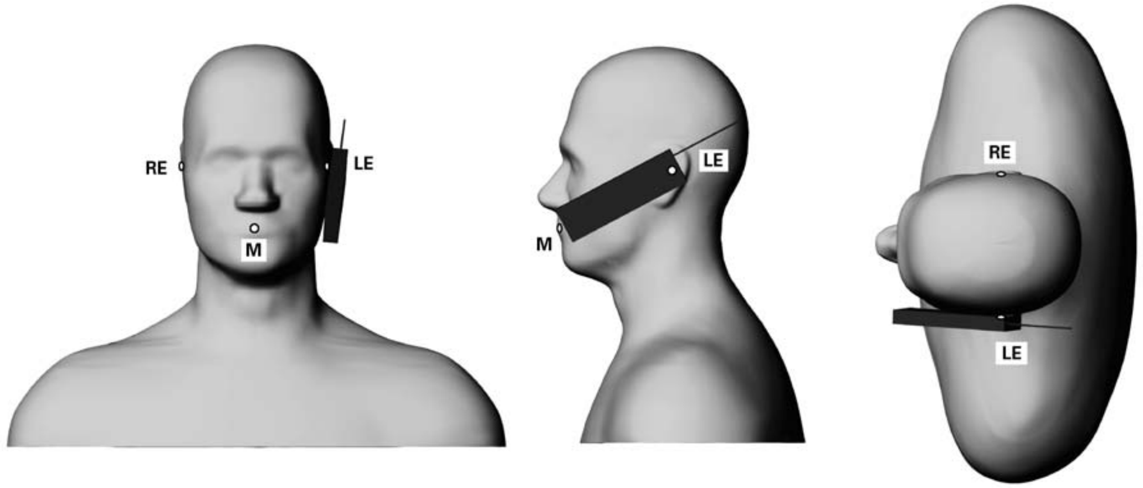


Figure 5.9.d. Phone position 1, "cheek" or "touch" position. The reference points for the right ear (RE), left ear (LE) and mouth (M), which define the reference plane for phone positioning, are indicated. The shoulders are shown for illustration purposes only.

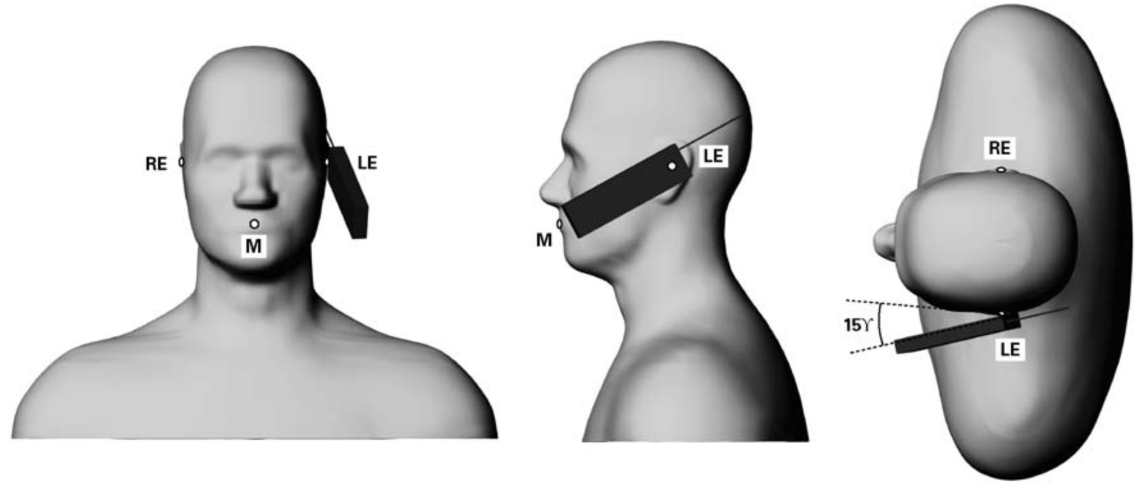


Figure 5.9.e. Phone position 2, "tilted position." The reference points for the right ear (RE), left ear (LE) and mouth (M), which define the reference plane for phone positioning, are indicated. The shoulders are shown for illustration purposes only.

5.10. SAR MEASUREMENT UNCERTAINTY

This uncertainty analysis covers the 3D-EMC Laboratory test procedure for Specific Absorption Rate (SAR) associated with wireless telephones and similar devices.

Standards Covered Are:

WGMTE 96/4 - Secretary SC211/B

FCC 96-326, ET Docket No. 93-62

Industry Canada RSS 102

ACA Radiocommunications (Electromagnetic Radiation – Human Exposure) Amendment Standard 2000 (No. 1)

The laboratory test procedure, and this uncertainty analysis, may be used to cover all standards above. It is based on test equipment and procedures specified by 3D-EMC Laboratories, Inc. located in Ft. Lauderdale, Florida.

5.10.1. Measurement Uncertainty

5.10.1.1. Measurement Uncertainty evaluation for handset SAR test

a	*b*	*c*	*d*	*e = f(d,k)*	*F*	*g*	*h = c x f / e*	*i = c x g / e*	*k*
Uncertainty Component	Sec.	**Tol. (± %)**	**Prob. Dist.**	**Div.**	**c_i (1-g)**	**c_i (10-g)**	**1-g u_i (±%)**	**10-g u_i (±%)**	v_i
Measurement System									
Probe Calibration	E1.1	3.0	N	1	1	1	3.0	3.0	∞
Axial Isotropy	E1.2	5.0	R	√3	0.7	0.7	2.0	2.0	∞
Hemispherical Isotropy	E1.2	8.0	R	√3	1	1	4.6	4.6	∞
Boundary Effect	E1.3	10.0	R	√3	1	1	5.8	5.8	∞
Linearity	E1.4	4.2	R	√3	1	1	2.4	2.4	∞
System Detection Limits	E1.5	2.0	R	√3	1	1	1.2	1.2	∞
Readout Electronics	E1.6	1.0	N	1	1	1	1.0	1.0	∞
Response Time	E1.7	1.5	R	√3	1	1	0.9	0.9	∞
Integration Time	E1.8	2.0	R	√3	1	1	1.2	1.2	∞
RF Ambient Conditions	E5.1	3.0	R	√3	1	1	1.7	1.7	∞
Probe Positioner Mechanical Tolerance	E5.2	1.0	R	√3	1	1	0.6	0.6	∞
Probe Positioning with respect to Phantom Shell	E5.3	3.0	R	√3	1	1	1.7	1.7	∞
Extrapolation, interpolation and Integration Algorithms for Max. SAR Evaluation	E4.2	3.5	R	√3	1	1	2.0	2.0	∞
Test sample Related									
Test Sample Positioning	E3.2.1	7.5	N	1	1	1	7.5	7.5	*11*
Device Holder Uncertainty	E3.1.1	6.5	N	1	1	1	6.5	6.5	*8*
Output Power Variation - SAR drift measurement	5.6.2	5.0	R	√3	1	1	2.9	2.9	∞
Phantom and Tissue Parameters									
Phantom Uncertainty (shape and thickness tolerances)	E2.1	4.0	R	√3	1	1	2.3	2.3	∞
Liquid Conductivity Target - tolerance	E2.2	5.0	R	√3	0.7	0.5	2.0	1.4	∞
Liquid Conductivity - measurement uncertainty	E2.2	4.0	R	√3	0.7	0.5	1.6	1.2	∞
Liquid Permittivity Target tolerance	E2.2	5.0	R	√3	0.6	0.5	1.7	1.4	∞
Liquid Permittivity - measurement uncertainty	E2.2	4.0	R	√3	0.6	0.5	1.4	1.2	∞
Combined Standard Uncertainty			RSS				14.3	14.2	
Expanded Uncertainty (95% confidence interval)							**28.5**	**28.3**	

5.10.1.2. *Measurement Uncertainty for System Performance Check*

a	*b*	*c*	*d*	*e = f(d,k)*	*f*	*g*	*h = c x f / e*	*i = c x g / e*	*k*
Uncertainty Component	**Sec.**	**Tol. (± %)**	**Prob. Dist.**	**Div.**	**c_i (1-g)**	**c_i (10-g)**	**1-g u_i (±%)**	**10-g u_i (±%)**	**v_i or v_{eff}**
Measurement System									
Probe Calibration	E1.1	3.0	N	1	1	1	3.0	3.0	∞
Axial Isotropy	E1.2	5.0	R	√3	0.7	0.7	2.0	2.0	∞
Hemispherical Isotropy	E1.2	8.0	R	√3	1	1	4.6	4.6	∞
Boundary Effect	E1.3	10.0	R	√3	1	1	5.8	5.8	∞
Linearity	E1.4	4.2	R	√3	1	1	2.4	2.4	∞
System Detection Limits	E1.5	2.0	R	√3	1	1	1.2	1.2	∞
Readout Electronics	E1.6	1.0	N	1	1	1	1.0	1.0	∞
Response Time	E1.7	1.5	R	√3	1	1	0.9	0.9	∞
Integration Time	E1.8	2.0	R	√3	1	1	1.2	1.2	∞
RF Ambient Conditions	E5.1	3.0	R	√3	1	1	1.7	1.7	∞
Probe Positioner Mechanical Tolerance	E5.2	0.4	R	√3	1	1	0.2	0.2	∞
Probe Positioning with respect to Phantom Shell	E5.3	3.0	R	√3	1	1	1.7	1.7	∞
Extrapolation, interpolation and Integration Algorithms for Max. SAR Evaluation	E4.2	3.5	R	√3	1	1	2.0	2.0	∞
Dipole									
Dipole Axis to Liquid Distance	7, X3.2	2.0	R	√3	1	1	1.2	1.2	∞
Input Power and SAR Drift Measurement	7, 5.6.2	3.0	R	√3	1	1	1.7	1.7	∞
Phantom and Tissue Parameters									
Phantom Uncertainty - shell thickness tolerance	E2.1	4.0	R	√3	1	1	2.3	2.3	∞
Liquid Conductivity – deviation from target values	E2.2	5.0	R	√3	0.7	0.5	2.0	1.4	∞
Liquid Conductivity - measurement uncertainty	E2.2	4.0	R	√3	0.7	0.5	1.6	1.2	∞
Liquid Permittivity – deviation from target values	E2.2	5.0	R	√3	0.6	0.5	1.7	1.4	∞
Liquid Permittivity - measurement uncertainty	E2.2	4.0	R	√3	0.6	0.5	1.4	1.2	∞
Combined Standard Uncertainty			RSS				10.0	9.9	
Expanded Uncertainty (95% confidence interval)							**20.1**	**19.8**	

EXHIBIT 6. SAR PRESCANS

6.1. BODY-WORN (BY STANDER) CONFIGURATION

6.1.1. Test configurations used

Body-worn (By Stander) operating configurations should be tested with the device positioned against a flat phantom in normal use configurations. The D.U.T. was placed against the phantom and tested in its appropriate configuration as would normally be used by the end user. If the SAR measured at the middle channel for each test is at least 3.0 dB lower than the SAR limit, testing at the high and low channels is optional for such test configuration(s).

If the transmission band of the test device is less than 10 MHz, testing at the high and low frequency channels is optional.

Body-worn accessories may not always be supplied or available as options for some devices that are intended to be authorized for body-worn use. A separation distance of 1.5 cm between the back of the device and a flat phantom is recommended for testing body-worn SAR compliance under such circumstances. Other separation distances may be used, but they should not exceed 2.5 cm. In these cases, the device may use body-worn accessories that provide a separation distance greater than that tested for the device provided however that the accessory contains no metallic components..

6.1.2. Equipment permutation investigated for each orientation

N/A

6.1.3. Comments on non-tested configurations

N/A

6.2. RECOMMENDED CAUTION STATEMENTS TO BE INCLUDED IN USERS MANUAL

In order for users to be aware of the body-worn operating requirements for meeting RF exposure compliance, operating instructions and caution statements should be included in the manual. The information should allow users to make informed decisions on the type of body-worn accessories and operating configurations that are appropriate for the device. The following are *examples* of typical statements that provide end-users with the necessary information about body-worn accessories:

Example 1. For a product that has the potential to be used in a body worn configuration and has been tested and certified with a specific accessory device(s):

“For body worn operation, this phone has been tested and meets the FCC RF exposure guidelines when used with the (*manufacturer name*) accessories supplied or designated for this product. Use of other accessories may not ensure compliance with FCC RF exposure guidelines. ”

Example 2. For a product that has the potential to be used in a body worn configuration and has not been certified with a specific accessory device(s):

“For body worn operation, this phone has been tested and meets FCC RF exposure guidelines when used with an accessory that contains no metal and that positions the handset a minimum of (specified distance) from the body. Use of other accessories may not ensure compliance with FCC RF exposure guidelines.”

Example 3. For a product that has the potential to be used in a body worn configuration with future manufacturer designed accessories:

“For body worn operation, this phone has been tested and meets the FCC RF exposure guidelines when used with a (*manufacturer name*) accessory designated for this product or when used with an accessory that contains no metal and that positions the handset a minimum of (specified distance) from the body.”