#### **HYUNDAI CALIBRATION & CERTIFICATION TECH. CO., LTD.**



PRODUCT COMPLIANCE DIVISION SAN 136-1, AMI-RI , BUBAL-EUP, ICHEON-SI, KYOUNGKI-DO, 467-701, KOREA TEL : +82 31 639 8518 FAX : +82 31 639 8525 www.hct.co.kr

# **CERTIFICATE OF COMPLIANCE (SAR EVALUATION)**

#### **AXESSTEL INC.**

6480 Weathers Place, Suite 300, San Diego, CA 92121

Date of Issue: January 15, 2007 Test Report No.: HCT-SAR07-0106 Test Site: HYUNDAI CALIBRATION & CERTIFICATION TECHNOLOGIES CO., LTD.



This wireless portable device has been shown to be capable of compliance for localized specific absorption rate (SAR) for uncontrolled environment/general population exposure limits specified in ANSI/ IEEE Std. C95.1- 2005 and had been tested in accordance with the measurement procedures specified FCC/OET Bulletin 65 Supplement C and IEEE Std. 1528-2003. (See Test Report).

I attest to the accuracy of data. All measurements reported herein were performed by me or were made under my supervision and are correct to the best of my knowledge and belief. I assume full responsibility for the completeness of these measurements and vouch for the qualifications of all persons taking them.

Hyundai C-Tech Co., Ltd. Certifies that no party to this application has been denied FCC benefits pursuant **to section 5301 of the Anti- Drug Abuse Act of 1998, 21 U.S. C. 853(a)** 

SOG

 **Report prepared by : Ki-Soo Kim** 

 **Manager of Product Compliance Team** 

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# **SAR MEASUREMENT REPORT**

# **1.1 SCOPE**

Environmental evaluation measurements of specific absorption rate 1 (SAR) distributions in emulated human head and body tissues exposed to radio frequency (RF) radiation from wireless portable devices for compliance with the rules and regulations of the U.S. Federal Communications Commission (FCC).2

### **1. 2 Applicant**



**<sup>1</sup>**Specific Absorption Rate (SAR) is a measure of the rate of energy absorption due to exposure to an RF transmitting source (wireless portable device).

**<sup>2</sup>**IEEE/ANSI Std. C95.1-2005 limits are used to determine compliance with FCC ET Docket 93-62.



## **2.1 INTRODUCTION**

The FCC has adopted the guidelines for evaluating the environmental effects of radio frequency radiation in ET Docket 93-62 on Aug. 6, 1996 to protect the public and workers from the potential hazards of RF emissions due to FCC-regulated portable devices.[1]

The safety limits used for the environmental evaluation measurements are based on the criteria published by the American National Standards Institute (ANSI) for localized specific absorption rate (SAR) in IEEE/ANSI C95.1-2005 Standard for Safety Levels with Respect to Human Exposure to Radio Frequency Electromagnetic Fields, 3 kHz to 300 GHz. (c) 1992 by the Institute of Electrical and Electronics Engineers, Inc., New York, New York 10017.[2] The measurement procedure described in IEEE/ANSI C95.3-1992 Recommended Practice for the Measurement of Potentially Hazardous Electromagnetic Fields - RF and Microwave[3] is used for guidance in measuring SAR due to the RF radiation exposure from the Equipment Under Test (EUT). These criteria for SAR evaluation are similar to those recommended by the National Council on Radiation Protection and Measurements (NCRP) in Biological Effects and Exposure Criteria for Radio frequency Electromagnetic Fields," NCRP Report No. 86 (c) NCRP, 1986, Bethesda, MD 20814.[4] SAR is a measure of the rate of energy absorption due to exposure to an RF transmitting source. SAR values have been related to threshold levels for potential biological hazards.

### **2.2 SAR Definition**

Specific Absorption Rate (SAR) is defined as the time derivative (rate) of the incremental energy (dU) absorbed by (dissipated in) an incremental mass (dm) contained in a volume element (dV) of a given density (r ). It is also defined as the rate of RF energy absorption per unit mass at a point in an absorbing body .

$$
S A R = \frac{d}{d t} \left( \frac{d U}{d m} \right) = \frac{d}{d t} \left( \frac{d U}{\rho d v} \right)
$$

**Figure 2. SAR Mathematical Equation** 

SAR is expressed in units of Watts per Kilogram (W/kg).

**SAR** where:

 $\sigma$ 

 $\rho$ 

E

 $\sigma E^2/\rho$ 

conductivity of the tissue-simulant material (S/m)  $\equiv$ 

- mass density of the tissue-simulant material (kg/m<sup>3</sup>)  $\equiv$
- $\equiv$ Total RMS electric field strength (V/m)

NOTE: The primary factors that control rate of energy absorption were found to be the wavelength of the incident field in relations to the dimensions and geometry of the irradiated organism, the orientation of the organism in relation to the polarity of field vectors, the presence of reflecting surfaces, and whether conductive contact is made by the organism with a ground plane.[4]



### **3.1 SAR MEASUREMENT SET-UP**

These measurements are performed using the DASY4 automated dosimetric assessment system. It is made by Schmid & Partner Engineering AG (SPEAG) in Zurich, Switzerland. It consists of high precision robotics system (Staubli), robot controller, Pentium III computer, near-field probe, probe alignment sensor, and the generic twin phantom containing the brain equivalent material. The robot is a six-axis industrial robot performing precise movements to position the probe to the location (points) of maximum electromagnetic field (EMF) (see Fig.3).

A cell controller system contains the power supply, robot controller, teach pendant (Joystick), and remote control, is used to drive the robot motors. The PC consists of the HP Pentium 4 3.0GHz computer with Windows XP system and SAR Measurement Software DASY4, A/D interface card, monitor, mouse, and keyboard. The Staubli Robot is connected to the cell controller to allow software manipulation of the robot. A data acquisition electronic (DAE) circuit performs the signal amplification, signal multiplexing, AD-conversion, offset measurements, mechanical surface detection, collision detection, etc. is connected to the Electro-optical coupler (EOC). The EOC performs the conversion from the optical into digital electric signal of the DAE and transfers data to the PC plug-in card.



Figure 3. HCT SAR Lab. Test Measurement Set-up

The DAE3 consists of a highly sensitive electrometer-grade preamplifier with auto-zeroing, a channel and gain-switching multiplexer, a fast 16 bit AD-converter and a command decoder and control logic unit. Transmission to the PC-card is accomplished through an optical downlink for data and status information and an optical uplink for commands and clock lines. The mechanical probe mounting device includes two different sensor systems for frontal and sidewise probe contacts. They are also used for mechanical surface detection and probe collision detection. The robot uses its own controller with a built in VME-bus computer. The system is described in detail in [5].



# **4.1 DASY4 E-FIELD PROBE SYSTEM**

### **4.2 ET3DV6 Probe Specification**





and the Phantom



Figure 5. ET3DV6 E-field Probe

The SAR measurements were conducted with the dosimetric probe ET3DV6, designed in the classical triangular configuration [5] and optimized for dosimetric evaluation. The probe is constructed using the thick film technique; with printed resistive lines on ceramic substrates. The probe is equipped with an optical mortifier line ending at the front of the probe tip. It is connected to the EOC box on the robot arm and provides an automatic detection of the phantom surface. Half of the fibers are connected to a pulsed infrared transmitter, the other half to a synchronized receiver. As the probe approaches the surface, the reflection from the surface produces a coupling from the transmitting to the receiving fibers. This reflection increases first during the approach, reaches a maximum and then decreases. If the probe is flatly touching the surface, the coupling is zero. The distance of the coupling maximum to the surface is independent of the surface reflectivity and largely independent of the surface to probe angle. The DASY4 software reads the reflection during a software approach and looks for the maximum using a 2 nd order fitting. The approach is stopped at reaching the maximum.



# **5. DESCRIPTION OF TEST POSITION 5.1 HEAD POSITION**

The device was placed in a normal operating position with the Point A on the device, as illustrated in following drawing, aligned with the location of the RE(ERP) on the phantom. With the ear-piece pressed against the head, the vertical center line of the body of the handset was aligned with an imaginary plane consisting of the RE, LE and M. While maintaining these alignments, the body of the handset was gradually moved towards the cheek until any point on the mouth-piece or keypad contacted the cheek. This is a cheek/touch position. For ear/tilt position, while maintain the device aligned with the BM and FN lines, the device was pivot against ERP back for 15º or until the device antenna touch the phantom. Please refer to IEEE SC-2 P1528 illustration below. Figure 5.1 Side view of the phantom







Figure 5.2 Handset vertical and horizontal reference lines



# **5.2 Body Holster/Belt Clip Configurations**

Body-worn operating configurations are tested with the belt-clips and holsters attached to the device and positioned against a flat phantom in a normal use configuration. A device with a headset output is tested with a headset connected to the device. Body dielectric parameters are used.

Accessories for Body-worn operation configurations are divided into two categories: those that do not contain metallic components and those that contain metallic components. When multiple accessories that do not contain metallic components are supplied with the device, the device is tested with only the accessory that dictates the closest spacing to the body. Then multiple accessories that contain metallic components are tested with each accessory. If multiple accessory share an identical metallic component (i.e. the same metallic belt-clip used with different holsters with no other metallic components) only the accessory that dictates the closest spacing to the body is tested.

Body-worn accessories may not always be supplied or available as options for some Devices intended to be authorized for body-worn use. In this case, a test configuration with a separation distance between the back of the device and the flat phantom is used.

For this test the EUT is

- $\Box$  Placed into the Body worn accessory and the accessory is positioned against the surface of the phantom in a normal operating position. (2mm separation phantom thickness)
- Since this EUT does not supply any body worn accessory to the end user a distance of 20 mm from the EUT back surface to the liquid interface is configured for the generic test.

: See the attachment file\_ ATT. P (SAR TEST SET-UP PHOTO)

Transmitters that are designed to operate in front of a person's face, as in push-to-talk configurations, are tested for SAR compliance with the front of the device positioned to face the flat phantom. For devices that are carried next to the body such as a shoulder, waist or chest-worn transmitters, SAR compliance is tested with the accessory(ies), Including headsets and microphones, attached to the device and positioned against a flat phantom in a normal use configuration.

In all cases SAR measurements are performed to investigate the worst-case positioning. Worstcase positioning is then documented and used to perform Body SAR testing.

# **6.1 E-FIELD PROBE CALIBRATION PROCESS**

### **6.2 E-Probe Calibration**

Each probe is calibrated according to a dosimetric assessment procedure described in [6] with an accuracy better than +/- 10%. The spherical isotropy was evaluated with the procedure described in [7] and found to be better than +/-0.25dB. The sensitivity parameters (NormX, NormY, NormZ), the diode compression parameter (DCP) and the conversion factor (ConvF) of the probe is tested.

The free space E-field from amplified probe outputs is determined in a test chamber. This is performed in a TEM cell for frequencies bellow 1 GHz, and in a waveguide above 1 GHz for free space. For the free space calibration, the probe is placed in the volumetric center of the cavity and at the proper orientation with the field. The probe is then rotated 360 degrees.

E-field temperature correlation calibration is performed in a flat phantom filled with the appropriate simulated brain tissue. The measured free space E-field in the medium correlates to temperature rise in a dielectric medium. For temperature correlation calibration a RF transparent thermistor-based temperature probe is used in conjunction with the E-field probe.

$$
\text{SAR} = C \frac{\Delta T}{\Delta t}
$$

where:

 $\Delta t$  = exposure time (30 seconds),

heat capacity of tissue (brain or muscle),  $C =$ 

 $\Delta T$  = temperature increase due to RF exposure.

SAR is proportional to  $\Delta T / \Delta t$ , the initial rate of tissue heating, before thermal diffusion takes place. Now it's possible to quantify the electric field in the simulated tissue by equating the thermally derived SAR to the E- field;



Figure 9. E-Field and Temperature Figure 10. E-Field and temperature

$$
\text{SAR} = \frac{\left|\mathbf{E}\right|^2 \cdot \sigma}{\rho}
$$

where:

 $=$  simulated tissue conductivity,  $\sigma$ 

 $\rho$  = Tissue density (1.25 g/cm<sup>3</sup> for brain tissue)



measurements at 900MHz[5] measurements at 1.8GHz [5]



### **6.3 Data Extrapolation**

The DASY4 software automatically executes the following procedures to calculate the field units from the microvolt readings at the probe connector. The first step of the evaluation is a linearization of the filtered input signal to account for the compression characteristics of the detector diode. The compensation depends on the input signal, the diode type and the DC-transmission factor from the diode to the evaluation electronics. If the exciting field is pulsed, the crest factor of the signal must be known to correctly compensate for peak power. The formula for each channel can be given as [8]:

$$
V_i = U_i + U_i^2 \cdot \frac{cf}{dcp_i}
$$
\nwith  $V_i$  = compensated signal of channel i (i=x,y,z)  
\n $U_i$  = input signal of channel i (i=x,y,z)  
\n $cf$  = crest factor of exciting field (DASY parameter)  
\ndcp<sub>i</sub> = diode compression point (DASY parameter)

= compensated signal of channel  $i$  ( $i = x, y, z$ )

From the compensated input signals the primary field data for each channel can be evaluated:

 $V_i$ 

with

E-field probes:

| $E_i$                          | $\frac{V_i}{Norm_i}$                          | Norm_i                                   | sensor sensitivity of channel i | (i = x,y,z) |       |
|--------------------------------|---|--|---------------------------------|-------------|-------|
| $E_i$                          | ConvF   | const                                    | const                           | const       | const |
| $\frac{V}{Norm_i} \cdot ConvF$ | ConvF   | = sensitivity of enhancement in solution |                                 |             |       |
| $E_i$                          | = electric field strength of channel i in V/m |  |                                 |             |       |

The RSS value of the field components gives the total field strength (Hermetian magnitude):

 $E_{\text{tot}} = \sqrt{E_x^2 + E_y^2 + E_x^2}$ 

The primary field data are used to calculate the derived field units.



The power flow density is calculated assuming the excitation field to be a free space field.

$$
P_{\text{pure}} = \frac{E_{\text{tot}}^2}{3770}
$$
 with 
$$
P_{\text{pure}} = \text{equivalent power density of a plane wave in W/cm}^2
$$

$$
E_{\text{tot}} = \text{total electric field strength in V/m}
$$



# **7.1 PHANTOM & EQUIVALENT TISSUES**

### **7.2 SAM Phantom**

The SAM Phantom is constructed of a fiberglass shell integrated in a wooden table. The shape of the shell is based on data from an anatomical study designed to determine the maximum exposure in at least 90% of all users [9][10]. It enables the dosimetric evaluation of left and right hand phone usage as well as body mounted usage at the flat phantom region. A cover prevents the evaporation of the liquid. Reference markings on the Phantom allow the complete setup of all predefined phantom positions and measurement grids by manually teaching three points in the robot.



Filling Volume **Volume Approx.** 30 liters Dimensions 810 x 1000 x 500 mm (H x L x W)

**Shell Thickness 2.0 mm Eigure 11. SAM Phantom Figure 11. SAM Phantom** 

#### **7.3 Brain & Muscle Simulating Mixture Characterization**

The brain and muscle mixtures consist of a viscous gel using hydrox-ethyl cellulose (HEC) gelling agent and saline solution (see Table 1). Preservation with a bacteriacide is added and visual inspection is made to make sure air bubbles are not trapped during the mixing process. The mixture is calibrated to obtain proper dielectric constant (permittivity) and conductivity of the desired tissue. The mixture characterizations used for the brain and muscle tissue simulating liquids are according to the data by C. Gabriel and G. Hartsgrove [11].

| Ingredients        | Frequency (MHz) |       |       |      |       |       |       |      |      |      |
|--------------------|-----------------|-------|-------|------|-------|-------|-------|------|------|------|
| (%by weight)       | 450             |       | 835   |      | 915   |       | 1900  |      | 2450 |      |
| <b>Tissue Type</b> | Head            | Body  | Head  | Body | Head  | Body  | Head  | Body | Head | Body |
| Water              | 38.56           | 51.16 | 41.45 | 52.4 | 41.05 | 56.0  | 54.9  | 40.4 | 62.7 | 73.2 |
| Salt (NaCl)        | 3.95            | 1.49  | 1.45  | 1.4  | 1.35  | 0.76  | 0.18  | 0.5  | 0.5  | 0.04 |
| Sugar              | 56.32           | 46.78 | 56.0  | 45.0 | 56.5  | 41.76 | 0.0   | 58.0 | 0.0  | 0.0  |
| <b>HEC</b>         | 0.98            | 0.52  | 1.0   | 1.0  | 1.0   | 1.21  | 0.0   | 1.0  | 0.0  | 0.0  |
| Bactericide        | 0.19            | 0.05  | 0.1   | 0.1  | 0.1   | 0.27  | 0.0   | 0.1  | 0.0  | 0.0  |
| Triton X-100       | 0.0             | 0.0   | 0.0   | 0.0  | 0.0   | 0.0   | 0.0   | 0.0  | 36.8 | 0.0  |
| <b>DGBE</b>        | 0.0             | 0.0   | 0.0   | 0.0  | 0.0   | 0.0   | 44.92 | 0.0  | 0.0  | 26.7 |

**Table 1. Composition of the Tissue Equivalent Matter**

### **7.4 Device Holder for Transmitters**

In combination with the SAM Phantom V4.0, the Mounting Device (POM) enables the rotation of the mounted transmitter in spherical coordinates whereby the rotation points is the ear opening. The devices can be easily, accurately, and repeatable positioned according to the FCC and CENELEC specifications. The device holder can be locked at different phantom locations (left head, right head, flat phantom).

Note: A simulating human hand is not used due to the complex anatomical and geometrical structure of the hand that may produced infinite number of configurations [10]. To produce the Worst-case condition (the hand absorbs antenna output power),



the hand is omitted during the tests. The set of the test of the t



# **8.1 SYSTEM SPECIFICATIONS**

### **8.2 Robotic System Specifications**



#### **Tissue Parameters**



# **9.1 MEASUREMENT PROCESS**

### **9.2 System Verification**

Prior to assessment, the system is verified to the ±10% of the specifications at 1900MHz, 2450MHz by using the system validation kit. (Graphic Plots Attached)



### **9.3 Dosimetric Assessment Setup**

The evaluation was performed with the following procedure:

- 1. The SAR value at a fixed location above the ear point was measured and was used as a reference value for assessing the power drop.
- 2. The SAR distribution at the exposed side of the head was measured at a distance of 3.9mm from the inner surface of the shell. The area covered the entire dimension of the head and the horizontal grid spacing was 20mm x 20mm. Based on this data, the area of the maximum absorption was determined by spine interpolation.
- 3. Around this point, a volume of 30mm x 30mm x 30mm was assessed by measuring 5 x 5 x 7 points. On this basis of this data set, the spatial peak SAR value was evaluated with the following procedure:
	- a. The data at the surface were extrapolated, since the center of the dipoles is 2.7mm away from the tip of the probe and the distance between the surface and the lowest measuring point is 1.2mm. The extrapolation was based on a least square algorithm [13]. A polynomial of the fourth order was calculated through the points in z-axes. This polynomial was then used to evaluate the points between the surface and the probe tip.
	- b. The maximum interpolated value was searched with a straight-forward algorithm. Around this maximum the SAR values averaged over the spatial volumes (1g or 10g) were computed using the 3D-Spline interpolation algorithm. The 3D-spline is composed of three one-dimensional splines with the "Not a knot" condition (in x,y, and z directions) [13][14]. The volume was integrated with the trapezoidal algorithm. One thousand points (10 x 10 x 10) were interpolated to calculate the average.
	- c. All neighboring volumes were evaluated until no neighboring volume with a higher average value was found. Origin Y<sub>-</sub>axis



#### **Fig. 10. SAR Measurement Point in Area Scan**

# **10.1 ANSI/ IEEE C95.1 - 2005 RF EXPOSURE LIMITS**



#### **Table 2. Safety Limits for Partial Body Exposure**

#### **NOTES:**

- \* The Spatial Peak value of the SAR averaged over any 1 gram of tissue (defined as a tissue volume in the shape of a cube) and over the appropriate averaging time.
- \*\* The Spatial Average value of the SAR averaged over the whole-body.
- **\*\*\*** The Spatial Peak value of the SAR averaged over any 10 grams of tissue (defined as a tissue volume in the shape of a cube) and over the appropriate averaging time.

**Uncontrolled Environments** are defined as locations where there is the exposure of individuals who have no knowledge or control of their exposure.

**Controlled Environments** are defined as locations where there is exposure that may be incurred by persons who are aware of the potential for exposure, (i.e.as a result of employment or occupation).

## **11.1 MEASUREMENT UNCERTAINTIES**

Measurement uncertainties in SAR measurements are difficult to quantify due to several variables including biological, physiological, and environmental. However, we estimate the measurement uncertainties in SAR to be less than 15-25 % [16].

According to ANSI/IEEE C95.3, the overall uncertainties are difficult to assess and will vary with the type of meter and usage situation. However, accuracy's of 1 to  $\pm$  3 dB can be expected in practice, with greater uncertainties in near-field situations and at higher frequencies (shorter wavelengths), or areas where large reflecting objects are present. Under optimum measurement conditions, SAR measurement uncertainties of at least  $\pm$  2dB can be expected.[3]

According to CENELEC [17], typical worst-case uncertainty of field measurements is 5 dB. For well-defined modulation characteristics the uncertainty can be reduced to  $\pm$  3 dB.



**Table 3. Breakdown of Errors** 

# **12.1 TEST CONFIGURATIONS**

### **SAR Testing with IEEE 802.11 a/b/g Transmitters**

Normal Network operating configurations are not suitable for measuring the SAR of 802.11 a/b/g transmitters. Unpredictable fluctuations in network traffic and antenna diversity conditions can introduce undesirable variations in SAR results. The SAR for these devices should be measured using chipset based test mode software to ensure the results are consistent and reliable.

#### **12. 2 General Device Setup**

Chipset based test mode software is hardware dependent and generally varies among manufacturers. The device operating parameters established in test mode for SAR measurements must be identical to those programmed in production units, including output power levels, amplifier gain settings and other RF performance tuning parameters. The test frequencies should correspond to actual channel frequencies defined for domestic use. SAR for devices with switched diversity should be measured with only one antenna transmitting at a time during each SAR measurement, according to a fixed modulation and data rate. The same data pattern should be used for all measurements.

#### **12. 3 General Device Setup**

80.11 a/b/g and 4.9 GHz operating modes are tested independently according to the service requirements in each frequency band. 80.211 b/g modes are tested on channels 1, 6 and 11.802.11a is tested for UNII operations on channels 36 and 48 in the 5.15-5.25 GHz band; channels 52 and 64 in the 5.25-5.35 GHz band; Channels 104, 116, 124 and 136 in the 5.470-5.725 GHz band; and channels 149 and 161 in the 5.8 GHz band. When 5.8 GHz § 15.247 is also available, channels 149, 157 and 165 should be tested instead of the UNII channels. 4.9 GHz is tested on channels 1, 10 and 5 or 6, whichever has the higher output power, for 5 MHz channels; channels 11,15 and 19 for 10 MHz channels; and channels 21 and 25 for 20 MHz channels.

These are referred to as the "default test channels". 802.11g mode was evaluated only if the output power was 0.25 dB higher than the 802.11b mode.



Table 4. **802.11 Test Channels per FCC Requirements**

# **13.1 3G MEASUREMENT PROCEDURES**

### **13. 2 Procedures Used To Establish Test Signal**

The handset was placed into a simulated call using a base station simulator in a shielded chamber. Such test signals offer a consistent means for testing SAR and are recommended for evaluating SAR. SAR measurements were taken with a fully charged battery. In order to verify that the device was tested and maintained at full power, this was configured with the base station simulator. The SAR measurement software calculates a reference point at the start and end of the test to check for power drifts. If conducted power deviations of more then 5% occurred, the tests were repeated.

### **13. 3 SAR Measurement Conditions for CDMA2000 1x**

These procedures were followed according to FCC "SAR Measurement Procedures for 3G Devices", May 2006.

### **13. 3. 1 Output Power Verification**

See 3GPP2 C.S0011/TIA-98-E as recommended by "SAR Measurement Procedures for 3G Devices", May 2006.

Maximum output power is verified on the High, Middle and Low channels according to procedures defined in section 4.4.5.2 of 3GPP2 C.S0011/TIA-98-E. SO55 tests were measured with power control bits in "All Up" condition.

- 1. If the mobile station supports Reverse TCH RC 1 and Forward TCH RC 1, set up a call using Fundamental Channel Test Mode 1 (RC=1/1) with 9600 bps data rate only.
- 2. Under RC1, C.S0011 Table 4.4.5.2-1 (Table 4) parameters were applied.
- 3. If the MS supports the RC 3 Reverse FCH, RC3 Reverse SCH0 and demodulation of RC 3, 4, or 5, set up a call using Supplemental Channel Test Mode 3 (RC 3/3) with 9600 bps Fundamental Channel and 9600 bps SCH0 data rate Channel and 9600 bps SCH0 data rate.
- 4. Under RC3, C.S0011 Table 4.4.5.2-2(Table 5) was applied.
- 5. FCHs were configured at full rate for maximum SAR with "All Up" power control bits.





Parameters for Max, Power for RC3



### **13. 3. 2 Head SAR Measurement**

SAR for head exposure configurations is measured in RC3 with the DUT configured to transmit at full rate using Loopback Service Option SO55. SAR for RC1 is not required when the maximum average output of each channel is less than ¼ dB higher than that measured in RC3. Otherwise, SAR is measured on the maximum output channel in RC1 using the exposure configuration that results in the highest SAR for that channel in RC3.



### **13. 3. 3 Body SAR Measurement**

SAR for body exposure configurations is measured in RC3 with the DUT configured to transmit at full rate on FCH with all other code channels disabled using TDSO / SO32. SAR for multiple code channels (FCH + SCHn) is not required when the maximum average output of each RF channel is less than ¼ dB higher than that measured with FCH only. Otherwise, SAR is measured on the maximum output channel (FCH + SCHn) with FCH at full rate and SCH0 enabled at 9600 bps using the exposure configuration that results in the highest SAR for that channel with FCH only. When multiple code channels are enabled, the DUT output may shift by more than 0.5 dB and lead to higher SAR drifts and SCH dropouts.

Body SAR in RC1 is not required when the maximum average output of each channel is less than  $\frac{1}{4}$ dB higher than that measured in RC3. Otherwise, SAR is measured on the maximum output channel in RC1; with Loopback Service Option SO55, at full rate, using the body exposure configuration that results in the highest SAR for that channel in RC3.

### **13. 3. 4 Handsets with EV-DO**

For handsets with Ev-Do capabilities, when the maximum average output of each channel in Rev. 0 is less than ¼ dB higher than that measured in RC3 (1x RTT), body SAR for Ev-Do is not required. Otherwise, SAR for Rev. 0 is measured on the maximum output channel at 153.6 kbps using the body exposure configuration that results in the highest SAR for that channel in RC3. SAR for Rev. A is not required when the maximum average output of each channel is less than that measured in Rev. 0 or less than <sup>1/4</sup> dB higher than that measured in RC3. Otherwise, SAR is measured on the maximum output channel for Rev. A using a Reverse Data Channel payload size of 4096 bits and a Termination Target of 16 slots defined for Subtype 2 Physical Layer configurations. A Forward Traffic Channel data rate corresponding to the 2-slot version of 307.2 kbps with the ACK Channel transmitting in all slots should be configured in the downlink for both Rev. 0 and Rev. A



#### **Average Output Power Measurement for FCC ID: PH7MV430**



# **13.1 SAR TEST DATA SUMMARY**



### 13.2 Measurement Results **(EVDO PCS CDMA Body SAR)**



NOTES:

1. The test data reported are the worst-case SAR value with the antenna-head position set in a typical configuration. Test procedures used are according to FCC/OET Bulletin 65, Supplement C [July 2001].

2. All modes of operation were investigated and the worst-case are reported.

3. Measured Depth of Simulating Tissue is 15.2 ± 0.2cm.

4. Tissue parameters and temperatures are listed on the SAR plot.

5. Battery Type  $\boxtimes$  Standard  $\Box$  Extended  $\Box$  Fixed, Batteries are fully charged for all readings.

- 6. Power Measured  **図 Conducted ロ EIRP** ERP
	-
- 7. SAR Configuration  $\Box$  Head  $\boxtimes$  Body  $\Box$  Hand
- 8. Test Signal Call Mode  $\Box$  Manual Test cord  $\boxtimes$  Base Station Simulator
- 9. Body SAR was tested under EVDO Rev. A RETAP mode.



# **13.1 SAR TEST DATA SUMMARY**



### 13.3 Measurement Results **(802.11b Module Body SAR)**



NOTES:

1. The test data reported are the worst-case SAR value with the antenna-head position set in a typical configuration. Test procedures used are according to FCC/OET Bulletin 65, Supplement C [July 2001].

2. All modes of operation were investigated and the worst-case are reported.

3. Measured Depth of Simulating Tissue is 15.2 ± 0.2cm.

4. Tissue parameters and temperatures are listed on the SAR plot.

5. Battery Type  $\boxtimes$  Standard  $\Box$  Extended  $\Box$  Fixed, Batteries are fully charged for all readings.

- 
- 6. Power Measured **⊠** Conducted **□ EIRP EERP**
- 
- 7. SAR Configuration 
<br>
□ Head 
<br>
<br>  $\boxtimes$  Body 
□ Hand
- 8. Test Signal Call Mode  $\boxtimes$  Manual Test cord  $\Box$  Base Station Simulator
	-



# **13.1 SAR TEST DATA SUMMARY**



### 13.3 Measurement Results **(802.11g Module Body SAR)**



NOTES:

- 1. The test data reported are the worst-case SAR value with the antenna-head position set in a typical configuration. Test procedures used are according to FCC/OET Bulletin 65, Supplement C [July 2001].
- 2. All modes of operation were investigated and the worst-case are reported.
- 3. Measured Depth of Simulating Tissue is 15.2 ± 0.2cm.
- 4. Tissue parameters and temperatures are listed on the SAR plot.
- 5. Battery Type  $\boxtimes$  Standard  $\Box$  Extended  $\Box$  Fixed, Batteries are fully charged for all readings.
- 
- 6. Power Measured **No. 2018** Conducted  $\Box$  EIRP ERP
- 
- 7. SAR Configuration  $\Box$  Head  $\boxtimes$  Body  $\Box$  Hand
- 8. Test Signal Call Mode <br> **EXA Manual Test cord** □ Base Station Simulator



# **14.1 SAR TEST EQUIPMENT**



#### NOTE:

The E-field probe was calibrated by SPEAG, by the waveguide technique procedure. Dipole Validation measurement is performed by HCT Lab. before each test. The brain simulating material is calibrated by HCT using the dielectric probe system and network analyzer to determine the conductivity and permittivity (dielectric constant) of the brain-equivalent material.



# **15.1 CONCLUSION**

The SAR measurement indicates that the EUT complies with the RF radiation exposure limits of the ANSI/ IEEE C95.1 2005.

These measurements are taken to simulate the RF effects exposure under worst-case conditions. Precise laboratory measures were taken to assure repeatability of the tests.





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