ENGINEERING TEST REPORT

ISL39001C Prism Duette PCMCIA Card
Model No.: ISL39001C

Tested For

Intersil Corporation
Rembrandtlaan 1a
3723 BG Bilthoven
P.O. Box 343
3720 AH Bilthoven
The Netherlands

In Accordance With

SAR (Specific Absorption Rate) Requirements
using guidelines established in IEEE C95.1-1991,
FCC OET Bulletin 65 (Supplement C),
Industry Canada RSS-102(Issue 1) and
ACA Radiocommunications (Electromagnetic Radiation – Human Exposure)
Amendment Standard 2000 (No. 1)

UltraTech's File No.: ITS-007-SAR

This Test report is Issued under the Authority of Tri M. Luu, Professional Engineer, Vice President of Engineering UltraTech Group of Labs Date: June 25, 2003	LICENSED PROFESSIONAL ENGINEER T.M. LUU PROVINCE OF ONTARIO
Report Prepared by: JaeWook Choi Issued Date: June 24, 2003	Tested by: JaeWook Choi Test Dates: June 18, 2003 ~ June 21, 2003

The results in this Test Report apply only to the sample(s) tested, which has been randomly selected.

UltraTech

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EXHIBIT 1. INTRODUCTION

1.1. SCOPE

Reference:	SAR (Specific Absorption Rate) Requirements IEEE C95.1-1991, FCC OET Bulletin 65 (Supplement C) Industry Canada RSS-102 (Issue 1). ACA Radiocommunications (Electromagnetic Radiation – Human Exposure), Amendment Standard 2000 (No. 1)
Title	Safety Levels with respect to human exposure to Radio Frequency Electromagnetic Fields Guideline for Evaluating the Environmental Effects of Radio Frequency Radiation
Purpose of Test:	To verify compliance with Federal regulated SAR requirements in Canada, Australia and the US.
Method of Measurements:	IEEE C95.1-1991, FCC OET Bulletin 65 (Supplement C) and Industry Canada RSS-102 (Issue 1)
Exposure Category	General Population/Uncontrolled

1.2. REFERENCES

The methods and procedures used for the measurements contained in this report are details in the following reference standards:

Publications	Year	Title
IEEE Std. 1528-2001 Draft	2001	Draft Recommended practice for determining the Peak Spatial-Average Specific Absorption rate (SAR) in the Human Body Due to Wireless Communications Devices: Experimental Techniques.
Industry Canada RSS102	1999	"Evaluation Procedure for Mobile and Portable Radio Transmitters with respect to Health Canada's Safety Code 6 for Exposure of Humans to Radio Frequency Fields"
ACA	2000	ACA Radiocommunications (Electromagnetic Radiation – Human Exposure) Amendment Standard 2000 (No. 1)
NCRP Report No.86	1986	"Biological Effects and Exposure Criteria for radio Frequency Electromagnetic Fields"
FCC OET Bulletin 65	1997	"Evaluating Compliance with FCC Guidelines for Human Exposure to radio Frequency Fields"
ANSI/IEEE C95.3	1992	"Recommended Practice for the Measurement of Potentially Hazardous Electromagnetic Fields - RF and Microwave"
ANSI/IEEE C95.1	1992	"Safety Levels with Respect to Human Exposure to Radio Frequency Electromagnetic Fields, 3kHz to 300GHz"
AS/NZS 2722.1	1998	Interim Australian/New Zealand Standard. "Radiofrequency fields, Part 1:Maximum exposure levels – 3kHz to 300GHz "

EXHIBIT 2. PERFORMANCE ASSESSMENT

2.1. CLIENT AND MANUFACTURER INFORMATION

APPLICANT:	
Name:	Intersil Corporation
Address:	Rembrandtlaan 1a 3723 BG Bilthoven P.O. Box 343 3720 AH Bilthoven The Netherlands
Contact Person:	Mr. Derick Sariredjo Phone #: +1-905-812-6200 Fax #: +1-905-812-6301 Email Address: derick.sariredjo@intersil.com

MANUFACTURER:	
Name:	Intersil Corporation
Address:	Rembrandtlaan 1a 3723 BG Bilthoven P.O. Box 343 3720 AH Bilthoven The Netherlands
Contact Person:	Mr. Derick Sariredjo Phone #: +1-905-812-6200 Fax #: +1-905-812-6301 Email Address: derick.sariredjo@intersil.com

2.2. DEVICE UNDER TEST (D.U.T.) DESCRIPTION

The following is the information provided by the applicant.

Trade Name	PRISM Duette
Type/Model Number	ISL39001C
Type of Equipment	Wireless LAN 802.11a/g adapter
Frequency of Operation	2412 MHz ~ 2462MHz (ISM-2.4 band) 5180 MHz ~ 5320 MHz (UNII-1, UNII-2 band)
Rated RF Power	18.9 dBm_{pk} conducted (ISM-2.4 band) 16.0 dBm_{pk} conducted (UNII-1 band) 19.0 dBm_{pk} conducted (UNII-2 band)
Modulation Employed	DSSS (ISM-2.4 band) OFDM (UNII band)
Antenna[*]	Skycross dual band PCB antenna (Gain: 1.65 dBi_{pk} at 2450 MHz, 3.1 dBi_{pk} at 5320 MHz)
Power Supply	Power supplied through the laptop computer
Primary User Functions of D.U.T.:	Data radio communication through air

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[*] Refer to EXHIBIT 11. manufacturer's declaration antenna assembly / configuration statement

2.3. LIST OF D.U.T.'S ACCESSORIES:

N/A

2.4. SPECIAL CHANGES ON THE D.U.T.'S HARDWARE/SOFTWARE FOR TESTING PURPOSES

N/A

2.5. ANCILLARY EQUIPMENT

Laptop computer (HP, M/N: HP OmniBook 6100, S/N: TW21607544, Card-to-Top: 5 mm, Card-to-Bottom: 8 mm)

2.6. GENERAL TEST CONFIGURATIONS

2.6.1. Equipment Configuration

Power and signal distribution, grounding, interconnecting cabling and physical placement of equipment of a test system shall simulate the typical application and usage in so far as is practicable, and shall be in accordance with the relevant product specifications of the manufacturer.

The configuration that tends to maximize the D.U.T.'s emission or minimize its immunity is not usually intuitively obvious and in most instances selection will involve some trial and error testing. For example, interface cables may be moved or equipment re-orientated during initial stages of testing and the effects on the results observed.

Only configurations within the range of positions likely to occur in normal use need to be considered.

The configuration selected shall be fully detailed and documented in the test report, together with the justification for selecting that particular configuration.

2.6.2. Exercising Equipment

The exercising equipment and other auxiliary equipment shall be sufficiently decoupled from the D.U.T. so that the performance of such equipment does not significantly influence the test results.

2.7. SPECIFIC OPERATING CONDITIONS

D.U.T. was mad to transmit with 100 % duty cycle, in other words continuously, instead of its actual duty cycle, using the exclusive controlling software for SAR test provided by the manufacturer.

2.8. BLOCK DIAGRAM OF TEST SETUP

The D.U.T. was configured as normal intended use. The following block diagram shows a representative equipment arrangement during tests:

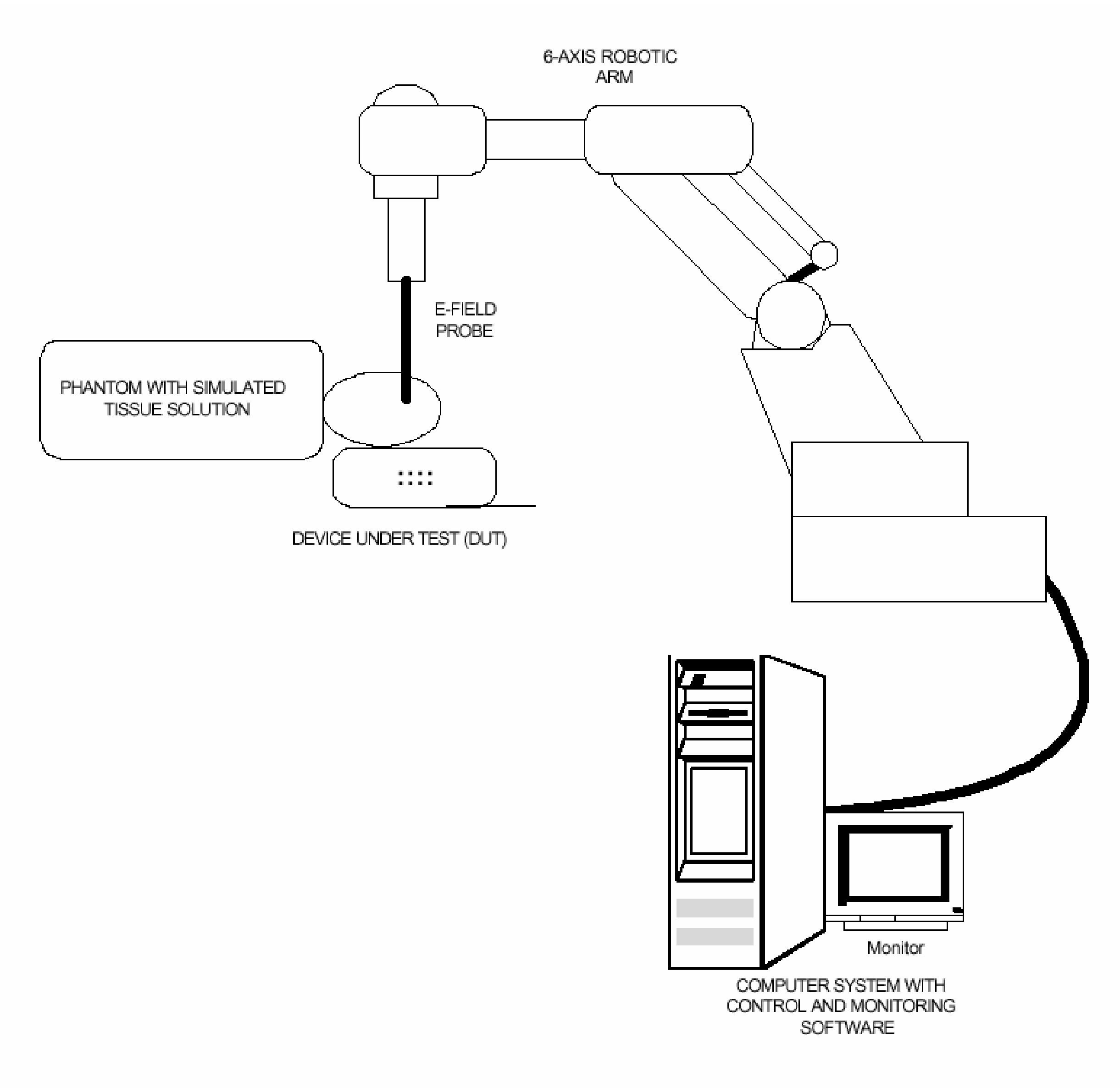

EXHIBIT 3. SUMMARY OF TEST RESULTS

3.1. LOCATION OF TESTS

All of the measurements described in this report were performed at UltraTech Group of Labs located at:

3000 Bristol Circle, in the city of Oakville, Province of Ontario, Canada.

All measurements were performed in UltraTech's shielded chamber, 24' x 16' x 8'.

3.2. APPLICABILITY & SUMMARY OF SAR RESULTS

The maximum peak spatial - average SAR measured was found to be 0.74 W/Kg.

Exposure Category and SAR Limits	Test Requirements	Compliance (Yes/No)
General population/Uncontrolled exposure 0.08W/kg whole body average and **spatial peak SAR of 1.6W/kg**, averaged over 1gram of tissue Hands, wrist, feet and ankles have a peak SAR not to exceed 4 W/kg, averaged over 10 grams of tissue.	Requirements using guidelines established in IEEE C95.1-1991 FCC OET Bulletin 65 (Supplement C) Industry Canada RSS-102 (Issue 1). ACA Radiocommunications (Electromagnetic Radiation – Human Exposure) Amendment Standard 2000 (No. 1)	YES
Occupational/Controlled Exposure 0.4W/kg whole body average and **spatial peak SAR of 8W/kg**, averaged over 1gram of tissue Hands, wrist, feet and ankles have a peak SAR not to exceed 20 W/kg, averaged over 10 grams of tissue.	Requirements using guidelines established in IEEE C95.1-1991 FCC OET Bulletin 65 (Supplement C), Industry Canada RSS-102 (Issue 1) ACA Radiocommunications (Electromagnetic Radiation – Human Exposure) Amendment Standard 2000 (No. 1)	N/A

EXHIBIT 4. MEASUREMENTS, EXAMINATIONS & TEST DATA

4.1. TEST SETUP

D.U.T. Information		**Condition**	
Product Name	ISL39001C Prism Duette PCMCIA Card	**Robot Type**	6 Axis
Model Number	ISL39001C	**Scan Type**	SAR – Area/Zoom/Att Vs Depth
Serial Number	3	**Measured Field**	E
Frequency Band [MHz]	2412 ~ 2462 (ISM-2.4) 5180 ~ 5320 (UNII-1, UNII-2)	**Phantom Type**	2_{mm} base Flat Phantom
Frequency Tested [MHz]	2437, 5260	**Phantom Position**	Waist
Rated RF Output Power [dBm]	18.9_{pk} conducted (ISM-2.4) 16.0_{pk} conducted (UNII-1) 19.0_{pk} conducted (UNII-2)	**Room Temperature** [°C]	23 ± 1
Antenna Type	Dual band PCB antenna	**Room Humidity** [%]	30 ± 10
Modulation	DSSS (ISM-2.4) OFDM (UNII)	**Tissue Temperature** [°C]	23 ± 1
Duty Cycle	100 %*		

Type of Tissue	Muscle	Muscle
Test Frequency [MHz]	2450	5240
Measured Dielectric Constant	54.3 (+3.0 %)	47.3 (-3.5 %)
Measured Conductivity [S/m]	1.96 (+0.5 %)	5.55 (+3.7 %)
Penetration Depth (Plane Wave Excitation) [mm]	20.1	6.7
Probe Model Number	E-TR	E-TR
Probe Serial Number	UT-0200-1	UT-0200-1
Probe Orientation	Isotropic	Isotropic
Probe Offset [mm]	2.00	2.00
Probe Tip Diameter [mm]	4.00	4.00
Sensor Factor (η_{pd}) [$mV/(mW/cm^2)$]	10.8	10.8
Conversion Factor (γ)	4.028	2.721
Sensitivity (ζ) [W/Kg/mV]	1.699E-01	7.120E-01

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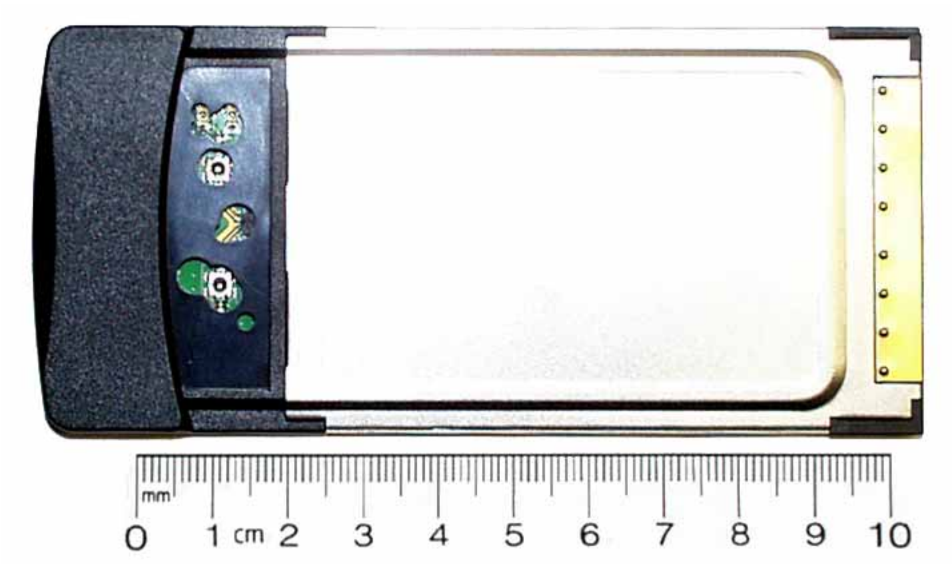
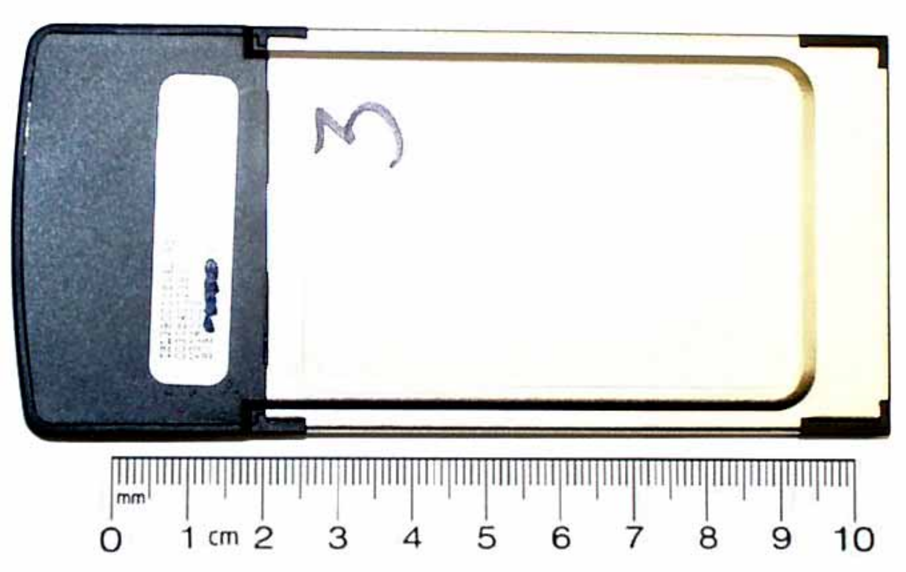
[*] Refer to 2.7

4.2. PHOTOGRAPH OF D.U.T. AND ALL ACCESORIES



< D.U.T. - Front view >



< D.U.T. - Rear view >

< Host laptop PC – HP OmniBook 6100 >

< E.U.T inserted into the bottom PC slot – Card-to-Bottom = 8 mm >

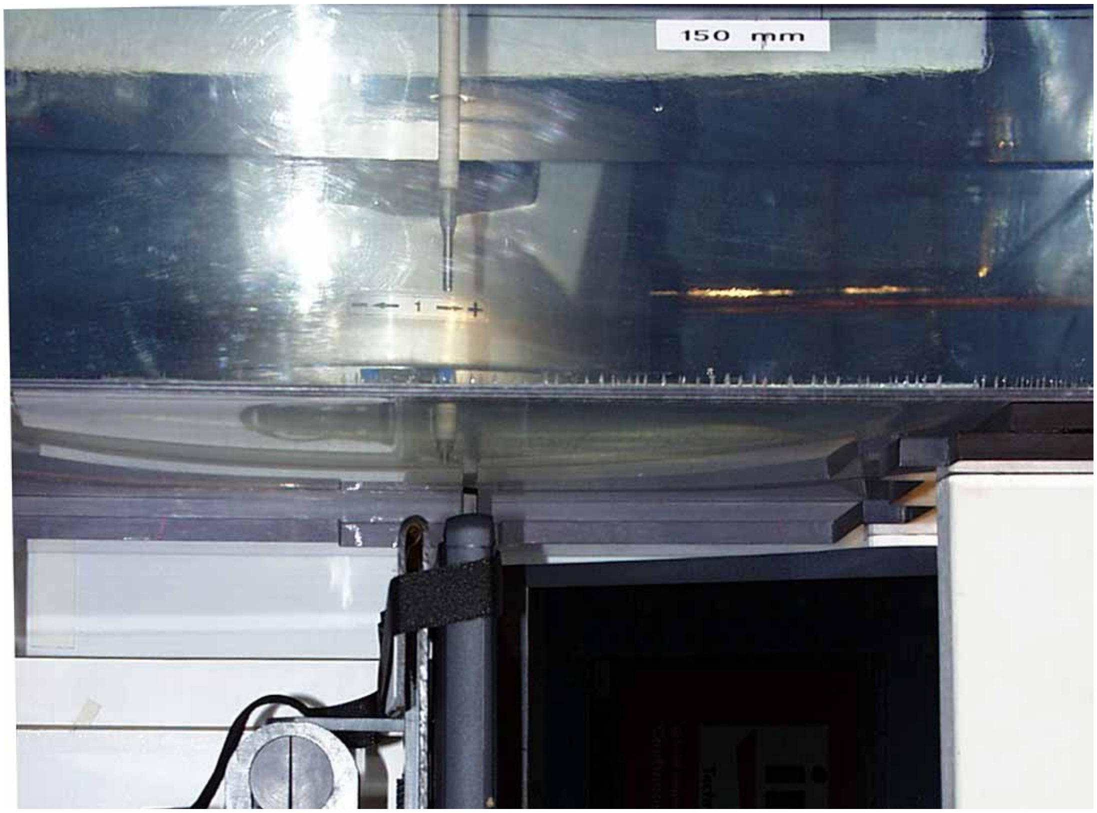
< E.U.T. inserted into the top PC slot – Card-to-Top = 5 mm >

4.3. PHOTOGRAPHS OF D.U.T. POSITION

4.3.1. Body Configuration

During the prescans, the minimum separation distance was determined for safety compliance. Since the different host laptop PCs have different dimensions (refer to 2.5.ANCILLARY EQUIPMENT), the separation distance between phantom and D.U.T. (Card) was specified by noting the gap between the top (or bottom) of the host PC and phantom as well as the distance between the card and the top (or bottom) of the host PC. α in the description of the photographs represented the gap between the top (or bottom) of the host PC and the phantom and it was varied to determine the minimum safety distance while the Card-to-Top (or Card-to-Bottom) distance was a fixed number and dependent on the host laptop PC used for testing. The various thickness of the Teflon pieces were used to maintain the distance α while testing.

< Bottom of the host PC faced toward the phantom (lap-top position) – 8 $_{mm}$(Card-to-Bottom) + α $_{mm}$>



< Edge of the card pointed toward the phantom (by-stander position) – α_{mm} >

< Top (Keyboard) of the host PC faced toward the phantom – 5 $_{mm}$(Card-to-Top) + α $_{mm}$ >

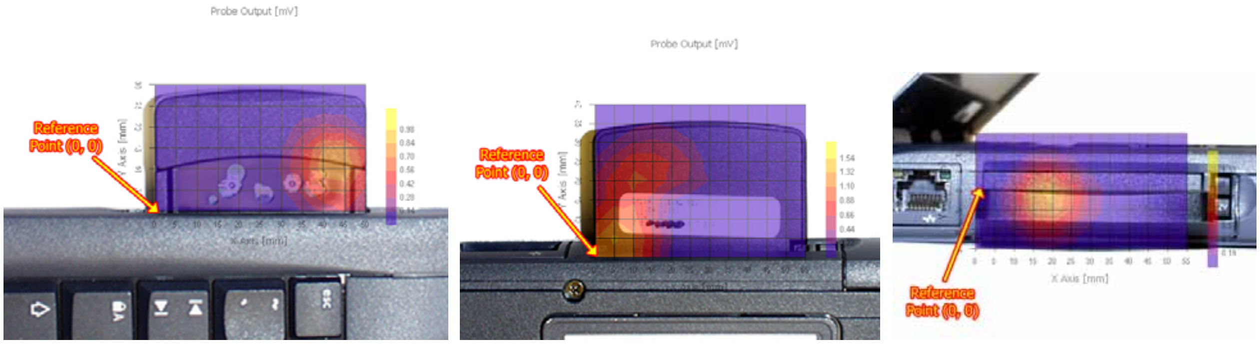
4.4. MAXIMUM PEAK SPATIAL-AVERAGE SAR

4.4.1. Maximum Peak Spatial-average SAR Data

#	Configuration	Device Test Positions	Antenna Position	Freq. [MHz]	Channel	MAX. 1g SAR [W/Kg]
05	UNII band, OFDM, 5260 MHz 9 Mbps data rate Bottom of the host PC faced toward the phantom, 8 mm (8 + 0) separation distance b/w the bottom surface of the card and the phantom (Host PC in contact with the phantom, card inserted into the bottom PC slot)	Body	Integrated	5260	52	0.74

4.4.2. Maximum Peak Spatial-Average SAR Location

Complete area prescan was conducted to determine the location of the highest SAR and the device was repositioned to allow the identified hot-spots to be orientated with as large an area around the hot-spots to come into contact with the phantom surface. This procedure ensured that the maximum SAR readings would be obtained from the hot-spot areas identified.



4.5. SAR MEASUREMENT DATA

4.5.1. Body Configuration Result[*]

4.5.1.1. 802.11g mode (ISM-2.4 band)

#	Configuration	Device Test Positions	Antenna Position	Freq. [MHz]	Channel	Ref. Local SAR Before [W/Kg]	Ref. Local SAR After [W/Kg]	MAX 1g SAR [W/Kg]
01	ISM-2.4 band, DSSS, 2437 MHz 1 Mbps data rate Bottom of the host PC faced toward the phantom, 8 mm (8 + 0) separation distance b/w the bottom surface of the card and the phantom (Host PC in contact with the phantom, card inserted into the bottom PC slot)	8 mm	Integrated	2412	01			
02		8 mm	Integrated	2437	06	0.10	0.09	0.22
03		8 mm	Integrated	2462	11			

4.5.1.2. 802.11a mode (UNII band)

#	Configuration	Device Test Positions	Antenna Position	Freq. [MHz]	Channel	Ref. Local SAR Before [W/Kg]	Ref. Local SAR After [W/Kg]	MAX 1g SAR [W/Kg]
04	UNII band, OFDM, 5260 MHz 9 Mbps data rate Bottom of the host PC faced toward the phantom, 8 mm (8 + 0) separation distance b/w the bottom surface of the card and the phantom (Host PC in contact with the phantom, card inserted into the bottom PC slot)	8 mm	Integrated	5180	36			
05		8 mm	Integrated	5260	52	0.80	0.78	0.74
06		8 mm	Integrated	5320	64			

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[*] If the SAR measured at the middle channel for each test configuration is at least 3.0 dB lower than the SAR limit, testing at the high and low channels is optional for such test configuration(s).

4.5.2. Power Measurement

4.5.2.1. 802.11g mode (ISM-2.4 band)

Bit rate [Mbps]	Measured RF conducted peak power [dBm]		
	CH 01, 2412 MHz	CH 06, 2437 MHz	CH11, 2462 MHz
1	17.7	18.3	18.1
2	17.7	18.3	18.1
5.5	17.1	18.2	18.0
11	17.5	18.2	18.1
9	18.4	18.5	17.3
18	18.7	18.5	18.1
36	188	18.9	18.5
54	18.8	18.8	18.7

4.5.2.2. 802.11a mode (UNII band)

Bit rate [Mbps]	Measured RF conducted peak power [dBm]			
	CH36, 5180 MHz	CH48, 5240 MHz	CH52, 5260 MHz	CH64, 5320 MHz
9	15.4	15.3	19.0	19.0
18	15.6	15.5	17.8	17.6
36	16.0	15.7	16.9	16.2
54	13.4	13.6	13.2	12.9

EXHIBIT 5. SAR SYSTEM CONFIGURATION & TEST METHODOLOGY

5.1. MEASUREMENT SYSTEM SPECIFICATIONS

Positioning Equipment	Probe
Type : 3D Near Field Scanner Location Repeatability : 0.1 [mm] Speed 180 [^{o}/sec] AC motors	Sensor : E-Field Spatial Resolution : 1 [mm^3] Isotropic Response : ±0.25 [dB] Dynamic Range : 0.01 to 100 [W/Kg]
Computer	**Phantom**
Type : Pentium III 500MHz Memory : 256 MB RAM Operating System : Windows 2000 Pro Monitor : 19" SVGA	Tissue : Simulated Tissue with electrical characteristics similar to those of the human at normal body temperature. Left/Right Head: IEEE P1528 Compliant SAM manufactured by Aprel Body/Frontal Head: IEEE Flat Phantom 2 $_{[mm]}$ Base

5.2. TEST PROCEDURES

In the SAR measurement, the positioning of the probes must be performed with sufficient accuracy to obtain repeatable measurements in the presence of rapid spatial attenuation phenomena. The accurate positioning of the E-field probe is accomplished by using a high precision robot. The robot can be taught to position the probe sensor following a specific pattern of points. In a first sweep, the sensor is positioned as close as possible to the interface, with the sensor enclosure touching the inside of the phantom shell. The SAR is measured on a grid of points, which covers the curved surface of the phantom in an area larger than the size of the D.U.T. After the initial scan, a high-resolution volume gird is used to locate the absolute maximum measured energy point and to calculate the peak spatial-average SAR. At this location, attenuation versus depth scan will be accomplished by the measurement system in order to verify the peak spatial-average SAR measured.

5.3. PHANTOM

For Head mounted devices placed next to the ear, the phantom used in the evaluation of the RF exposure of the user of the wireless device is a IEEE P1528 compliant SAM phantom, shaped like a human head and filled with a mixture simulating the dielectric characteristics of the brain. A left sided head and a right sided head are evaluated to determine the worst case orientation for SAR. For body mounted and frontal held push-to-talk devices, a flat phantom of dimensions 70x42x20cm with a base plate thickness of 2mm is used.

5.4. SIMULATED TISSUE

Simulated Tissue: Suggested in a paper by George Hartsgrove and colleagues in University of Ottawa Ref.: Bioelectromagnetics 8:29-36 (1987)

Ingredient	Quantity
Water	40.4 %
Sugar	56.0 %
Salt	2.5 %
HEC	1.0 %
Bactericide	0.1 %

Table 5.4. Example of composition of simulated tissue

This simulated tissue is mainly composed of water, sugar and salt. At higher frequencies, in order to achieve the proper conductivity, the solution does not contain salt. Also, at these frequencies, D.I. water and alcohol is preferred.

Target Frequency	Head		Body	
(MHz)	ε_r	σ (S/m)	ε_r	σ (S/m)
150	52.3	0.76	61.9	0.80
300	45.3	0.87	58.2	0.92
450	43.5	0.87	56.7	0.94
835	41.5	0.90	55.2	0.97
900	41.5	0.97	55.0	1.05
915	41.5	0.98	55.0	1.06
1450	40.5	1.20	54.0	1.30
1610	40.3	1.29	53.8	1.40
1800 – 2000	40.0	1.40	53.3	1.52
2450	39.2	1.80	52.7	1.95
3000	38.5	2.40	52.0	2.73
5240	35.9	4.70	49.0	5.35
5800	35.3	5.27	48.2	6.00

(ε_r = relative permittivity, σ = conductivity and ρ = 1000 Kg/m^{3*})

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[*] The actual mass density of the equivalent tissue vary based on the composition of the tissue from 990 Kg/m^3 to 1,300 Kg/m^3.

5.4.1. Preparation

The weight requirements is determined and measured carefully for all the components. A clean container is used where the ingredients will be mixed. A stirring paddle mounted to a drill press is used to stir the mixture. First the heat is applied to the DI water to approximately 40 ^{o}C to help the ingredients dissolve well and then the salt and the bactericide are added. It is stirred until all the ingredients are completely dissolved. It is continuously stirred slowly while adding the sugar. Rotation of stirring paddle at a high RPM is avoided to prevent air bubbles in the mixture. Later on, the HEC is added to maintain the solution homogeneous. Mixing time is approximately 2 hours.

5.5. MEASUREMENT OF ELECTRICAL CHARACTERISTICS OF SIMULATED TISSUE

1) Slotted Coaxial Waveguide
2) HP Dielectric Strength Probe System

5.5.1. Slotted Coaxial Waveguide

5.5.1.1. Equipment set-up

The test equipment consists of a slotted coaxial transmission line with a probe connected to a vector network analyzer, as shown in Figure 4.5.1.1. The log-magnitude and phase of S_{21} should be displayed simultaneously. Source power should be set to a level high enough to provide good signal-to-noise ratio. Periodically (annually or whenever the measuring scale along the line length is changed) a measurement is made on a reference liquid to validate the system. Since the measured quantities are magnitude and phase changes versus distance, the accuracy of the scale is very critical.

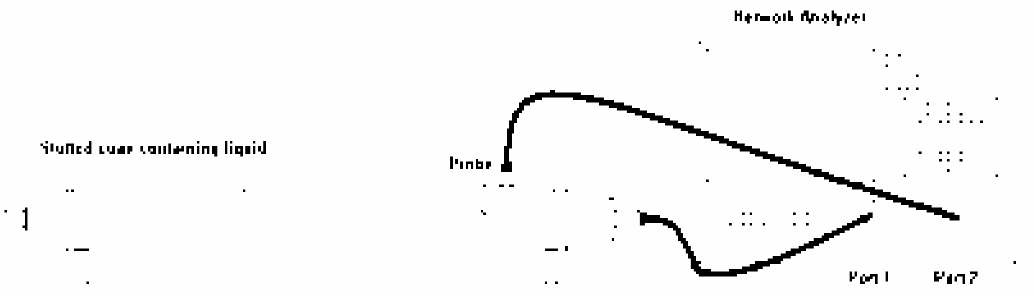

Figure 5.5.1.1. Slotted line set-up

The network analyzer injects a signal into one end of the slotted coaxial transmission line. The probe inserted through the slot into the tissue-equivalent material detects the RF amplitude and phase for each measurement position along the length of the line. A full two-port calibration of the network analyzer should be carried out prior to connecting the sample holder, and the following precautions should be observed:

a) Fill the slotted line carefully to avoid trapping air bubbles. This operation should be performed while the slotted line is horizontal.

b) The probe should be inserted into the slot at the end nearest to the input connector of the slotted line, ensuring that the tissue-equivalent liquid is flush with the inside surface of the line, and aligned with a well-defined position on the distance scale of the slotted line.

c) The probe should be inserted perpendicular to the slotted–line longitudinal axis until a stable and adequate amplitude response is achieved. Do not insert the probe too deeply into the coaxial line, because it can overly perturb the field distribution.

5.5.1.2. Measurement procedure.

a) Configure and calibrate the network analyzer.

b) Measure 10 to 20 log-magnitude and phase data points along the slotted line corresponding to about a 30 dB change in magnitude.

c) Plot S_{21} log-magnitude and phase vs. measurement distance.

d) Determine if the graphed points closely follow a straight-line approximation, based on the correlation coefficient or a similar statistical measure. The data should produce a good linear curve fit (expected correlation coefficient $r^2 > 0.99$ for lossy materials). If not, re-measure the liquid by increasing the sample points to extend the magnitude change from 30 to 40 dB. Note: for low loss materials, ensure that the slotted line is long enough to avoid reflections from the load-terminated end.

e) Calculate the conductivity and relative permittivity of the tissue-equivalent material using Equations (5.5.1.2.) derived from

$$
\begin{aligned}
\overline{\alpha} &= \frac{m_m \ln(10)}{20} && \text{Np/cm} \\
\overline{\beta} &= \frac{m_p \pi}{180} && \text{rad/cm} \\
\varepsilon_r' &= \frac{(\overline{\beta})^2 - (\overline{\alpha})^2}{\omega^2 \mu_0 \varepsilon_0} \\
\sigma &= \frac{2\overline{\alpha}\,\overline{\beta}}{\omega \varepsilon_0}\left(\frac{100\ \text{cm}}{\text{m}}\right) && \text{S/m}
\end{aligned}
\tag{5.5.1.2.}
$$

where, m_m and m_p are the slopes of the least-squares linear fits of the log-magnitude and phase plots, respectively, and $\overline{\alpha}$ and $\overline{\beta}$ are the average attenuation and propagation coefficients along the line.

5.5.2. HP Dielectric Strength Probe System (open-ended coaxial transmission-line probe/sensor)

5.5.2.1. Equipment set-up

The equipment consists of a probe connected to one port of a vector network analyzer. The probe is an open-ended coaxial line, as shown in Figure B.2. Cylindrical coordinates (ρ, ϕ, z) are used where ρ is the radial distance from the axis, ϕ is the angular displacement around the axis, z is the displacement along the axis, a is the inner conductor radius, and b is the outer conductor inner radius.

The sample holder is a non-metallic container that is large compared with the size of the probe immersed in it. A probe with an outer diameter *b* of 2 to 4 mm is suitable for the measurement of tissue-equivalent materials in the 300 MHz to 3 GHz frequency range. This probe size is commensurate with sample volumes of 50 cc or higher. Larger probes of up to 7 mm outer diameter *b* may be used with larger sample volumes. A flange is typically included to better represent the infinite ground-plane assumption used in admittance calculations.

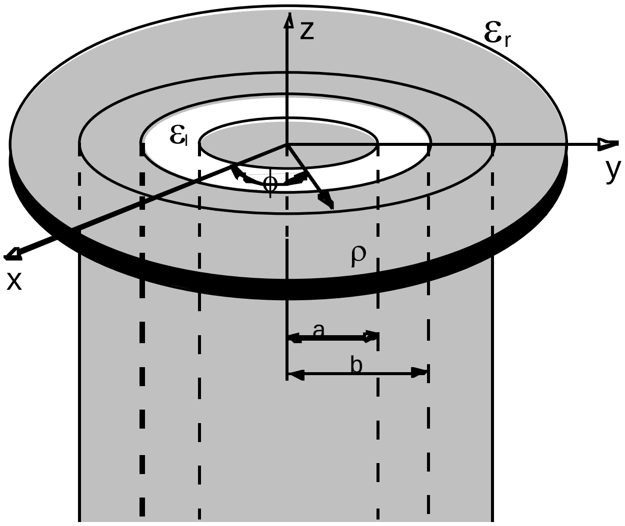

Figure 5.5.2.1. An open-ended coaxial probe with inner and outer radii *a* and *b*, respectively

The accuracy of the short-circuit measurement should be verified for each calibration at a number of frequencies. A short circuit can be achieved by gently pressing a piece of aluminum foil against the open end. For best electrical contact, the probe end should be flat and free of oxidation. Larger the sensors generally have better foil short-circuit repeatability. It is possible to obtain good contact with some commercial 4.6 mm probes using the metal-disk short-circuit supplied with the kit. For best repeatability, it may be necessary to press the disk by hand.

The network analyzer is configured to measure the magnitude and phase of the admittance. A one-port reflection calibration is performed at the plane of the probe by placing materials for which the reflection coefficient can be calculated in contact with the probe. Three standards are needed for the calibration, typically a short circuit, air, and de-ionized water at a well-defined temperature (other reference liquids such as methanol or ethanol may be used for calibration). The calibration is a key part of the measurement procedure, and it is therefore important to ensure that it has been performed correctly. It can be checked by re-measuring the short circuit to ensure that a reflection coefficient of $\Gamma = -1.0$ (linear units) is obtained consistently.

5.5.2.2. Measurement procedure

a) Configure and calibrate the network analyzer and probe system.

b) Place the sample in a non-metallic container and immerse the probe. A fixture or clamp is recommended to stabilize the probe, mounted such that the probe face is at an angle with respect to the liquid surface to minimize trapped air bubbles beneath the flange.

c) Measure the complex admittance with respect to the probe aperture.

d) Compute the complex relative permittivity $\varepsilon_r = \varepsilon_r' - j\,\sigma/\omega\varepsilon_0$.

5.6. SYSTEM CALIBRATION

The SAR measurement system has two main components:

a) the probe, which is connected to the inputs of
b) the instrumentation amplifier whose outputs are connected through the optical transmission line to
c) the computer.

The system is calibrated as one unit not as individual components. If any components is modified or replaced, the system must be re-calibrated.

The system calibration is performed by two steps:

1) determination of the sensitivity of the probe in the air by introducing it into the well-defined RF field, and
2) correlation of the measured E-field in the dielectric medium to the temperature rise in a dielectric medium.

5.6.1. Probe linearity

Detector diodes at the dipole feed-point are used to rectify the sensor voltage output. The rectified signal is transmitted through resistive (RF-transparent) lines to the sensor amplifier. At low field strength levels the output voltage is proportional to the square of the amplitude of the incident field; at higher signal levels, the output voltage is not linearly proportional to $|E|^2$, but becomes proportional to E. The compensation for diode compression is carried out for the each detector diode using the 3-rd order polynomial least-square fit algorithm before any further evaluation.

5.6.2. Free Space Calibration

Note: Equipment must be regularly calibrated.

- RF Signal Generator - frequency range to at least 6 GHz,
- RF Amplifier – if needed to generate the required power density in the test cell,
- Test Cell - TEM (Crawford) cell, waveguide, or other device capable of maintaining a uniform field,
- RF Power Meter - capable of measuring at least 5 Watts (current calibration is mandatory!) if possible traceable to the National Institute of Standards and Technology (NIST).
- E-Field Probe (under calibration)
- Probe Support Fixture
- Instrumentation Amplifier
- Transmission Line
- Computer Program with the Automated Calibration System Program

5.6.2.1. Method

Due to impedance variations in the diodes and the transmission line, and slight differences in gain among the channels of the instrumentation amplifier, a normalization method had been designed. The calibration method actually used is to determine the factors necessary adjust each channel of the system so it’s indicated output can then be equated to the well-defined RF field. These factors are referred to as “Amplifier Settings”.

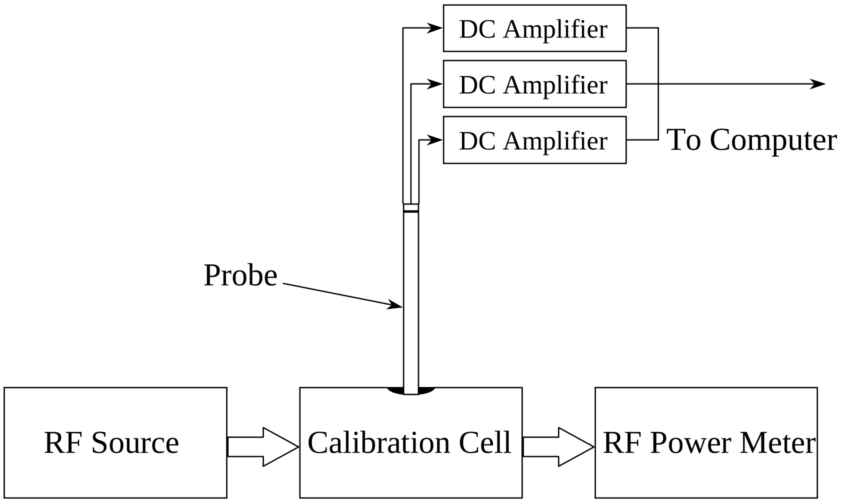

Figure 5.6.2.1. Free Space Calibration Setup for Amplifier Setting

5.6.2.2. Measurement procedure

Free Space Calibration of E-field probes can be performed using a TEM cell manufactured by IFI (Instrumentation for Industry, Farmingdale, NY 11735) with operating frequency at or below 1 GHz. Above 1 GHz, waveguides are used to calibrate the probes in free space.

- Connect the equipments as shown in Figure 5.6.2.1;
- Adjust the RF generator output so that the power density at the calibration point inside the TEM cell is well-defined. (For the IFI model CC-110 cell, the uniform power density of 1.0 [mW/cm^2] requires the power level of 271.0 [mW]);
- Mount the probe of the system to calibrate in the support fixture. Insert the probe through the aperture of the TEM cell. The probe handle should be at the geometric center of the aperture, i.e. midway between the septum and the upper surface, and orthogonal to the side of the cell. The sensing portion of the probe should be located at a point halfway across the depth of the cell (volumetric center).
- Once the prescribed position is obtained, it must be maintained during the rest of the measurement. The only movement of the probe allowed is rotation on its axis to position the dipole in the plane of the E-field and, for channel 3 only, parallel to the vertical uniform field (max./min. output).
- Verify that the RF power level remains constant throughout the measurement. While the probe is being rotated through 360 degrees, software indicators will show the maximum measured on each channel.

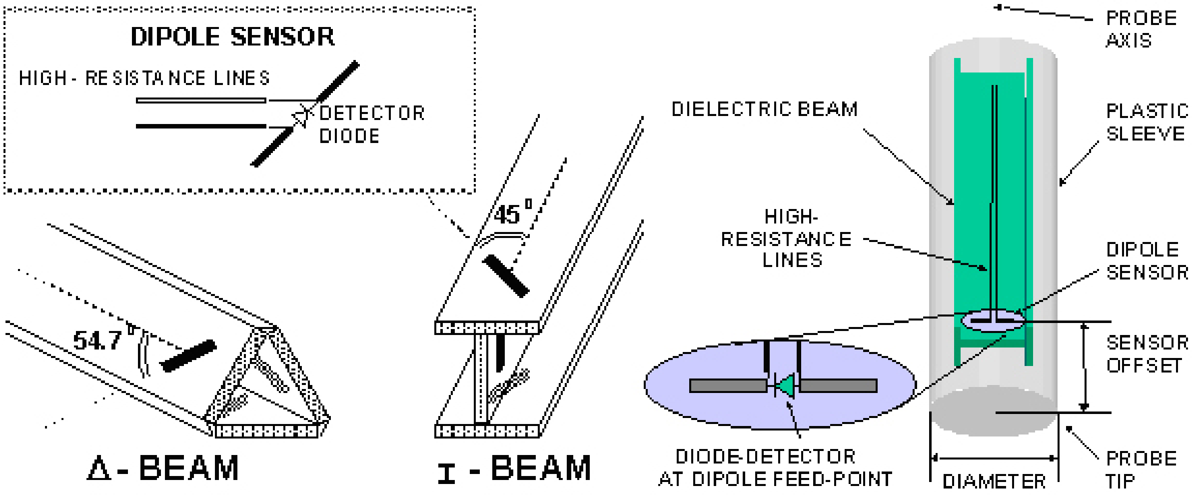

Figure 5.6.2.2. E-field probe construction

5.6.2.3. *Definition of Amplifier Settings*

The initial sequence of probe calibrations steps performed with SAR determinations produces the factors used in scaling probe output voltage to RF power density. For historical reasons all probes factors are compared to a factor 10.8 [mV] per [mW/cm^2] that was typical of a prototype probe, but is in fact an arbitrary number used as an intermediately constant. The factor of 10.8 [mV/(mW/cm^2)] is known as the sensor factor to the uniform power density (η_{pd}), but does not change. Also we can derive 10.8/3,770 [mV/(V/m)^2] of the sensor factor to the $|E|^2$ (η_{E2}), providing 377 [Ω] as free space impedance.

$$\eta_{Pd} = 10.8[mV/(mW/cm^2)] \equiv \eta_{E2} = \frac{10.8}{3770}[mV/(V/m)^2]$$

$$Pd[mW/cm^2] = \frac{PO_{tot}}{\eta_{Pd}}, \quad |E|^2[(V/m)^2] = \frac{PO_{tot}}{\eta_{E2}} \quad \text{and} \quad SAR = \frac{\sigma \times \frac{PO_{tot}}{\eta_{E2}}}{\rho}$$

To calibrate a probe, each channel is assigned an amplifier setting. This factor is obtained from the maximum probe output voltage measured during probe calibration. This probe output voltage is corrected for any DC offset of the instrumentation amplifier, usually a very small amount.

During calibration, the sensitivity for the E-field tangential to the dipole axis caused by the geometry of the probe construction is carefully considered to obtain the correct amplifier setting for each channel. Thus, the amplifier settings for each channel are as follows:

$$AS_i = \frac{\eta_{Pd}}{V_{\max_i} - DC_i} \times \cos^2(\varphi - \theta_i) \times Pd$$

Where,

AS_i	Amplifier Setting for channel i
η_{pd}	Sensor Factor to the uniform power density, an arbitrary value 10.8 [mV/(mW/cm^2)]
V_{maxi}	Maximum probe raw output recorded for channel i by rotation about the probe axis with the probe in a test cell
DC_i	Ambient DC offset of channel i (the voltage output of the transmission line with the instrumentation amplifier on and RF power off, recorded at the beginning of the probe calibration)
φ	Smaller angle between the probe axis and the direction of the E-field (90° providing the probe axis is parallel to the plane of the septum inside TEM cell)
θ_i	Smaller angle between the probe axis and the dipole sensor axis of the channel i ($\theta_1 = \theta_2 = 45°$, $\theta_3 = 90°$ for I-beam probe, and $\theta_1 = \theta_2 = \theta_3 = 54.7°$ for triangular-beam probe)
Pd	Well-defined power density [mW/cm^2] at the calibration point in a test cell

5.6.3. Thermal Transfer Calibration

5.6.3.1. Measurement procedure

An RF transparent thermistor-based temperature probe and a isotropic E-field probe are placed side-by-side in a planar phantom while both are exposed to RF energy from a half wave dipole antenna located below the phantom The E-field probe and amplifiers were previously calibrated.

First, the location of the maximum E-field close to the phantom's bottom is determined as a function of power into the dipole

Then, the E-field probe is moved sideways so that the temperature probe, while affixed to the E-field probe is placed at the previous location of the E-field probe.

Finally, temperature changes for a certain amount of time (generally 10 to 30 seconds) exposures at the same RF power levels used for the E-field are recorded. Care is taken to allow cooling down to the original temperature and temperature stabilization between tests.

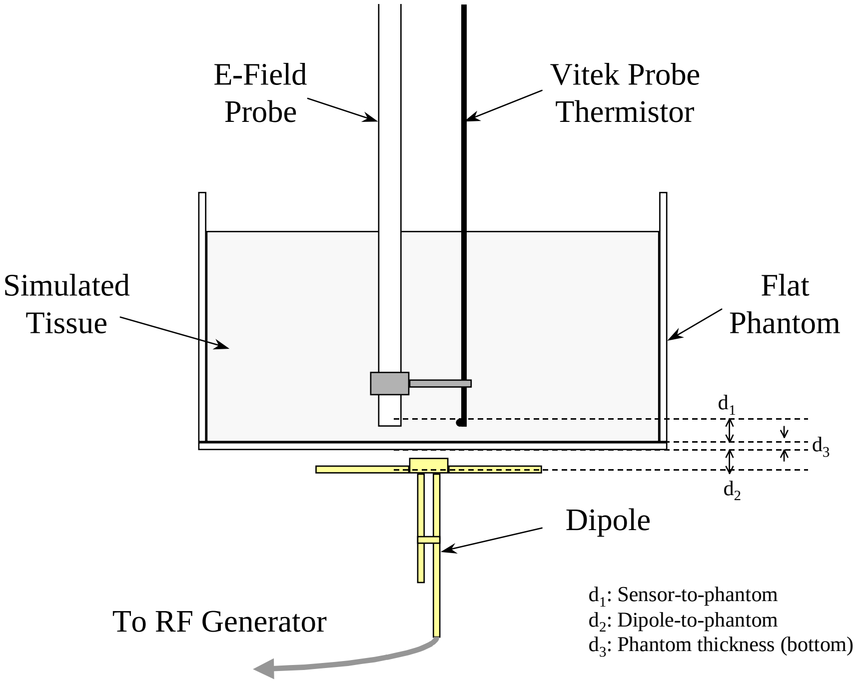

Figure 5.6.3.1. Flat Phantom, Thermistor and E-Field Probe

The following simple equation relates SAR to the initial temperature slope:

$$SAR_t = \frac{c \cdot \Delta T}{\Delta t} \qquad \text{(Eq. 1)}$$

In (Eq.1) Δt is the exposure time [sec], c is the specific heat capacity of the simulated tissue [J/Kg/ ^{o}C] and ΔT is the temperature increase [^{o}C] due to the RF exposure. SAR is proportional to ΔT/Δt, the initial rate of tissue heating, before thermal diffusion takes place.

From (Eq.1) it is possible to quantify the electric field in the simulated tissue by equating the thermally-derived SAR to the E-field:

$$SAR = \frac{|E|^2 \cdot \sigma}{\rho} \qquad \text{(Eq. 2)}$$

where σ is the simulated tissue conductivity [S/m] andρ its mass density [Kg/m^3]; The actual mass density of the simulated tissue is required during the thermal transfer calibration, while mass density of 1,000 [Kg/m^3] is conventionally chosen during the SAR measurements.

5.6.3.2. Determination of Conversion Factor (γ) in the simulated tissue

The sensitivity of the probe in the dielectric media compared to its sensitivity in the air, is different. Conversion Factor (γ) is defined to determine the degree of the enhancement of sensitivity in the different dielectric media and relate it to its sensitivity in the air.

$$PO_{tot\_tissue} \equiv PO_{tot\_air} \times \gamma$$

Thus,

$$\left|E_{tissue}\right|^2 = \frac{PO_{tot\_tissue}}{\eta_{E2}} \times \frac{1}{\gamma} \quad \text{,and} \quad SAR_{tissue} = \frac{\sigma \times \dfrac{PO_{tot\_tissue}}{\eta_{E2}} \times \dfrac{1}{\gamma}}{\rho}$$

where,

$\lvert E_{tissue}\rvert^2$	RMS E-field level [(V/m)^2] induced within the exposed tissue
PO_{tot_tissue}	Probe voltage output measured in the simulated tissue [mV]
PO_{tot_air}	Probe voltage output measured in the air (Z_{air} = 377[Ω]) [mV]
η_{E2}	Sensor Factor to the $\lvert E\rvert^2$, an arbitrary value 10.8/3,770 [mV/(V/m)^2]
γ	Conversion factor; ratio of sensor response in air to response in the dielectric media

The conversion factor (γ) can be used to scale the E-field in terms of the thermally-derived SAR. It is the quotient of SAR_t, the SAR determined from temperature measurements in the flat phantom, and PO_{tot_tissue}, the E-field prove output voltage obtained at the same location in the phantom

$$SAR_t = SAR_{tissue}$$

$$\frac{c \cdot \Delta T}{\Delta t} = \frac{\sigma_{@cal} \times \left|E_{tissue}\right|^2}{\rho}$$

$$= \frac{\sigma_{@cal} \times \dfrac{PO_{tot\_tissue}}{\eta_{E2}} \times \dfrac{1}{\gamma}}{\rho}$$

Thus,

$$\gamma = \frac{\sigma_{@cal}}{\eta_{E2} \times \rho} \times \frac{PO_{tot\_tissue}}{SAR_t} = \frac{\sigma_{@cal} \times 3{,}770}{10.8 \times c \times \rho} \times \frac{PO_{tot\_tissue}}{\Delta T / \Delta t} \qquad \text{(Eq. 3)}$$

where,

γ	Conversion factor; ratio of sensor response in air to response in the dielectric media
SAR_t	Thermally-derived SAR [W/Kg] (Eq. 1)
$\|E_{tissue}\|^2$	RMS E-field level [$(V/m)^2$] induced within the exposed tissue
PO_{tot_tissue}	Probe voltage output measured in the simulated tissue [mV]
η_{E2}	Sensor Factor to the $\|E\|^2$, an intermediately constant, 10.8/3,770 [$mV/(V/m)^2$]
c	Specific heat capacity of the simulated tissue [J/Kg/ ^{o}C]
$\sigma_{@cal}$	Conductivity of the simulated tissue during the calibration procedure [S/m]
ρ	Actual mass density of the simulated tissue [Kg/m^3]
$\Delta T/\Delta t$	Initial rate of tissue heating, before thermal diffusion takes place [^{o}C /sec]

The temperature E-field correlation is illustrated below (for simulated brain tissue) for an example in which the thermal quantities were,

RF power input = 0.5 [W]
$\Delta T = 0.0163$ [^{o}C] (from thermistor-base temperature probe)
$\sigma_{@cal} = 0.97$ [S/m]
$\rho = 1{,}200$ [Kg/m^3]
$c = 2{,}700$ [$J/Kg/^oC$]
$\Delta t = 30$ [sec]

The resulting SAR_t was (Eq. 1)

$$SAR_t = \frac{2{,}700 \times 0.0163}{30} = 1.467 \text{ [W/Kg]}$$

In this case the output of the E-field probe when at the same position as the thermistor probe was

$$PO_{tot\_tissue} = 210.93 \text{ [mV]}$$

The calculation of conversion factor (γ) from (Eq. 3) follows:

$$\gamma = \frac{0.97}{\frac{10.8}{3{,}770} \times 1{,}200} \times \frac{28.5}{1.467} = 5.482$$

5.6.4. Data Acquisition Methodology

5.6.4.1. E-Field Measurement

The probe calibration must be current before starting measurements. Instrumentation amplifier batteries must be charged. This can be monitored by observing DC offset voltages. A daily log of the DC offset voltages should be kept for this purpose.

Measurements in the phantom are automatically calculated for each location by summation of the three dipole outputs. Because each dipole produces an output voltage proportional to the square of the electric field component along the dipole, the sum of dipole voltages represents the RMS values for the total electric field. Thus, taking into consideration the amplifier settings and the DC offset voltages, the total electric field strength at a measurement location is as follows.

See Appendix C. PO_{tot} is labeled by the software as measure of values (voltages). The SAR for calculations that are derived from the measure of values are discussed below.

At each measurement point, the program records the output of the three channels:

$$PO_1 = (V_1 - DC_1) \times AS_1 \equiv |E_1|^2 \times \eta_{E2}$$
$$PO_2 = (V_2 - DC_2) \times AS_2 \equiv |E_2|^2 \times \eta_{E2}$$
$$PO_3 = (V_3 - DC_3) \times AS_3 \equiv |E_3|^2 \times \eta_{E2}$$

$$\begin{aligned} PO_{tot} &\equiv |E|^2 \times \eta_{E2} = \left(|E_1|^2 + |E_2|^2 + |E_3|^2\right) \times \eta_{E2} = |E_1|^2 \times \eta_{E2} + |E_2|^2 \times \eta_{E2} + |E_3|^2 \times \eta_{E2} \\ &\equiv PO_1 + PO_2 + PO_3 \end{aligned}$$

Where,

V_i	Actual raw reading of channel i at a measurement point
DC_i	Ambient DC offset of channel i at a measurement point
AS_i	Amplifier setting of channel i
η_{E2}	Sensor Factor to the $|E|^2$, an arbitrary value 10.8/3,770 [mV/(V/m)^2]
PO_i	Probe output of channel i at a measurement point [mV]
PO_{tot}	Total probe output at a measurement point [mV]

5.6.4.2. *Sensitivity(ζ) of probe in the simulated tissue*

The sensitivy(ζ) of the probe in the simulated tissue is rendered in terms of Sensor Enhancement Factor in the simulated tissue.

$$\zeta = \frac{\sigma_{@\,meas}}{\eta_{E2} \times \rho \times \gamma} = \frac{\sigma_{@\,meas}}{\frac{10.8}{3{,}770} \times 1{,}000 \times \gamma} = \frac{3{,}770 \times \sigma_{@\,meas}}{10{,}800 \times \gamma} \qquad \text{(Eq. 5)}$$

Where,

ζ	Sensitivity of the probe in the simulated tissue [W/Kg/mV]
γ	Conversion factor; ratio of sensor response in air to response in the dielectric media
η_{E2}	Sensor Factor to the $|E|^2$, an arbitrary value 10.8/3,770 [mV/(V/m)^2]
$\sigma_{@meas}$	Conductivity of the simulated tissue during the measurement [S/m]
ρ	Mass density of the simulated tissue [Kg/m^3]; 1,000 [Kg/m3] is conventionally chosen.

Therefore, SAR can be yielded from

$$SAR = \zeta \times PO_{tot\_tissue} \qquad \text{(Eq. 6)}$$

Where,

ζ	Sensitivity of the probe in the simulated tissue [W/Kg/mV]
PO_{tot_tissue}	Probe voltage output measured in the simulated tissue [mV]

To continue the example illustrated above,

$\sigma_{@meas} = 0.99$ [S/m]
$PO_{tot\_tissue} = 11.5$ [mV]

$$\zeta = \frac{3{,}770 \times \sigma_{@\,meas}}{10{,}800 \times \eta} = \frac{3{,}770 \times 0.99}{10{,}800 \times 5.482} = 0.063 \text{ [W/Kg/mV]}$$

$$SAR = \zeta \times PO_{tot\_tissue} = 0.063 \times 11.5 = 0.725 \text{ [W/Kg]}$$

5.6.4.3. SAR Measurement

The goal of the measurement process is to scan the phantom over a selected area in order to find the region of highest levels of RF energy and then to obtain a single value for the peak spatial-average of SAR over a volume that would contain one gram (in the shape of a cube) of biological tissue. The test procedure, of course, measures SAR in the simulated tissue.

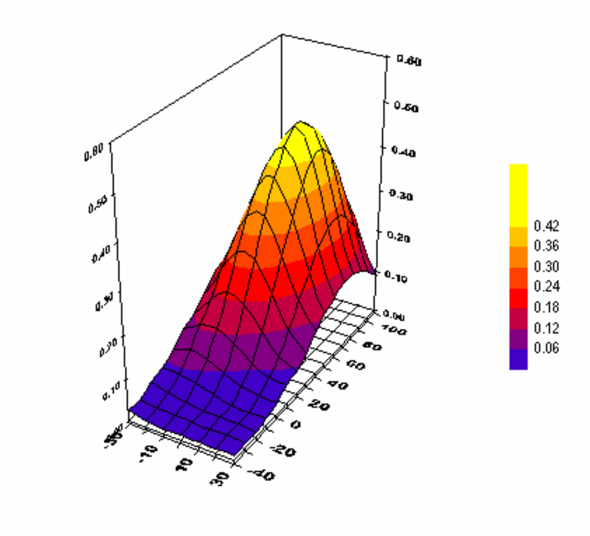

Figure 5.6.4.3.a. Area scan

The software request the user to move the probe to locations at two extreme corners of a rectangle that encloses the area to be scanned. An arbitrary origin and the spatial resolution for the scan are also specified. Under program control, the scan is performed automatically by the robot-guided probe.

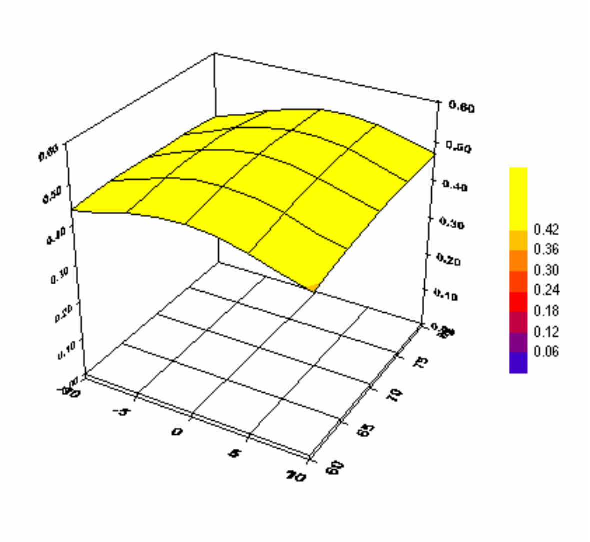

Figure 5.6.4.3.b. Zoom Scan

The fine resolution volume scan region is centered at the peak SAR locations determined by the interpolated (cubic spline) data from the area scan measurements. The number of measurement point required in a zoom scan is defined to provide an accurate one-gram averaged SAR in terms of both the number of points ($PT_X \times PT_Y \times PT_Z$) and the size ($SZ_X$[mm] × SZ_Y[mm] × SZ_Z[mm]) of the cubic. For one-gram SAR, (5 × 5 × 7) and (32[mm] × 32[mm] × 30[mm]) is preferred to select below 1 GHz. The zoom scan region extends in each direction for at least 1.5 times the linear dimensions of 1- or 10-gram cube of tissue from each peak. The zoom scan spatial resolution is interpolated down to SAR values on a 1mm grid by using the tri-linear interpolation algorithm.

The peak field values near the surface of a homogeneous phantom are usually not measurable because the sensors in a field probe are located at 2-4 mm behind the tip of the probe and the measurement point is defined at the geometric center of the sensors where the calibration is defined. These SAR values are computed by extrapolating the closest measured points to the surface of the phantom to determine the highest one-gram averaged SAR. The extrapolation coefficients are determined with a multi-order curve-fitting algorithm. Generally the 4-th order polynomial least-square fit is sufficient to extrapolate to the surface if the number of the valid measurements, that are non-zero, along the probe axis is greater than 4.

The interpolated and extrapolated SAR values from the zoom scan measurements are integrated in the shape of 1- or 10-gram cube then traversed to determine the highest peak spatial-average SAR in the zoom scan region.

This peak spatial-averaged SAR is reported as SAR [W/kg] for compliance.

5.6.4.4. Data Extrapolation and boundary effect

The distance from the center of the sensor (diode) to the end of the protective tube is called the ‘probe offset’ or ‘sensor offset’. To compensate we use a multi-order polynomial least-square curve fitting to obtain the peak surface value from the voltages measured at the distance from the inner surface of the phantom. The field is measured as close as possible to the phantom’s surface and every pre-defined separation distance (1 [mm] to 5 [mm]) along the probe axis (z) for a distance of at least 50 mm until they are not measurable. The appropriate curve is obtained from all the points measured and used to define an exponential decay of the energy density versus depth.

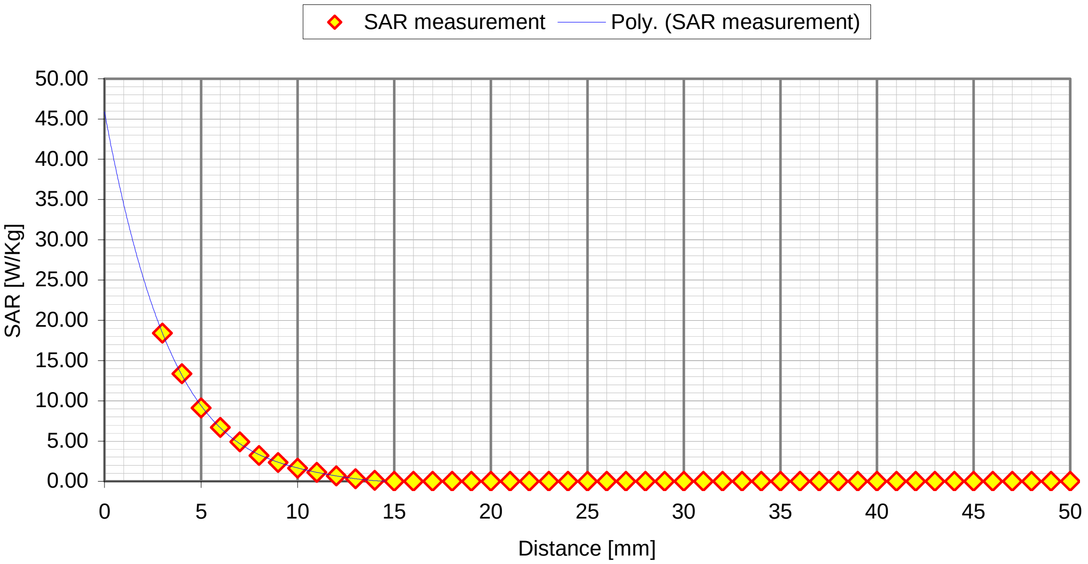

Figure 5.6.4.4. Exponential decay of the energy density versus depth

Boundary effects arise when the tip of an electric field probe approaches the interface between two dielectric media. Under these conditions, the external field is strongly perturbed by the superposition of a scattered field from the probe. The effect of the boundary on the peak spatial-average SAR values strongly depends on the probe dimensions, especially the diameter of the tip of the probe. It is known that the error due to boundary effects is very small if the distance between the probe tip and the surface is greater than half the probe diameter. Therefore the first one or two measurements at the vicinity to the phantom surface are excluded for evaluating the exponential decay curve in order to compensate for the boundary effect.

5.6.5. Determining the Heat Capacity of Simulated Tissue

5.6.5.1. Instruments and Materials

- Calibrated differential thermometer (Vitek or BAT-8 or equivalent)
- Two identical 500 ml containers
- A thermally insulated vessel (thick styrofoam, with a form fitting hole for one container)
- Hot and cold tap water
- Solution under test
- Hot plate
- Temperature vs. time (chart recorder, or data loger)

5.6.5.2. Method

Heat can be propagated by conduction, convection and radiation. In the case of liquids heated from below, gravity convection is the main and predominant heating mechanism of the fluid mass.

Obtain two containers that can be rapidly heated (e.g. glass or suitable plastic). Fill one container with 250 ml of water, the other with the same mass of simulated tissue. The initial temperature of the water should be the same as that of the simulated tissue (±1°C). Since we are dealing with heating by electromagnetic sources at ambient temperature, it is essential that we eliminate the chance of any direct infrared heating of the temperature sensor. To ensure this, position the tip of the sensor 2 mm from the bottom of the center of the container. Turn on the heat source and wait at least 5 minutes for its temperature to stabilize. Record the initial temperature of the water. Place the container of water 5 mm above the center of the hot plate and monitor the temperature increase.

After 30 seconds of heating, the water temperature should have increased by at least 5 °C. Record the time and temperature. Remove the container from the heat source and place it in the thermally insulated vessel. Stir the liquid thoroughly and record the steady state temperature 1-2 minutes after stirring.

Repeat the above procedure using the container of simulated tissue. Ensure that the container is placed on the same area of the hot plate, is heated for the identical length of time, and the steady state temperature is recorded after the identical time interval.

Since the heat capacity of water is C_w = 1,000 [cal/Kg/°C] or 4,189 [J/Kg/°C] with excellent approximation (~1%) in the temperature range of interest, the heat capacity (C_s) of the solution is given by:

$$C_s = C_w \cdot \frac{\Delta T_w}{\Delta T_s}$$

where ΔT_w is the temperature increase of water and ΔT_s the temperature increase of the solution. The ration of the values, $\Delta T_w / \Delta T_s$, should be the same (within the sensitivity of the thermometer) at the end of the heating and stirring. This ensures that the liquids have been uniformly heated.

5.6.5.3. Rationale

$$C \cdot \Delta T = Heat\_Flow \cdot Time = Total\_Heating\_Energy$$

If the heat flow, sample mass, and absorption (heat transfer) are the same for both liquids, then:

$$C_w \cdot \Delta T_w = C_s \cdot \Delta T_s$$

The heat flow and total heating are kept constant by using the same source for the same amount of time. If the heat transfer mechanisms for the woe liquids are about the same, with insignificant differences in convective and conductive characteristics, then any differences in temperature increase are a direct measure of the specific heat capacity, C.