

SECTION 4

PHOTOGRAPHS



4.1 TEST POSITIONAL PHOTOGRAPHS

OET65(c) HEAD PHANTOM TEST POSITIONS



Figure 59. Positional photograph of the Intermec 700C Left Hand Cheek Touch Position

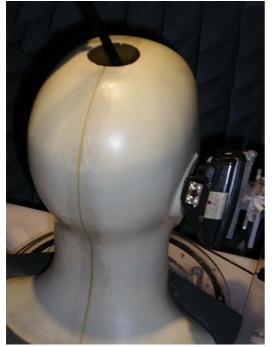


Figure 61. Positional photograph of the Intermec 700C Right Hand Cheek Touch Position



Figure 60. Positional photograph of the Intermec 700C Left Hand Cheek 15° Position



Figure 62. Positional photograph of the Intermec 700C Right Hand Cheek 15° Position



4.1 TEST POSITIONAL PHOTOGRAPHS

OET65(c) FLAT PHANTOM TEST POSITIONS – INTENDED and ALTERNATIVE



Figure 63. Positional photograph of the Intermec 700C Normal user position holster 1



Figure 64. Positional photograph of the Intermec 700C Normal user position holster 1

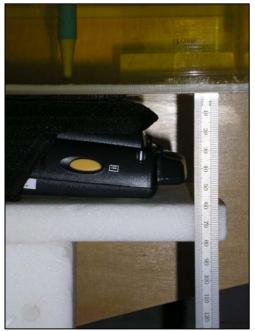


Figure 65. Positional photograph of the Intermec 700C Inverted position holster 1 rear facing



4.1 TEST POSITIONAL PHOTOGRAPHS - Continued

OET65(c) FLAT PHANTOM TEST POSITIONS – INTENDED and ALTERNATIVE

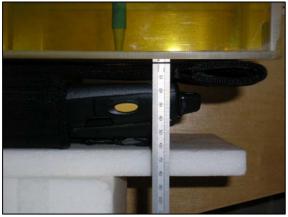


Figure 66. Positional photograph of the Intermec 700C Normal user position holster 2



Figure 67. Positional photograph of the Intermec 700C Inverted position holster 2



Figure 68. Positional photograph of the Intermec 700C Inverted position holster 2 (rear facing)



Figure 69. Positional photograph of the Intermec 700C Left Hand Side position holster 2



Figure 70. Positional photograph of the Intermec 700C Right Hand Side position holster 2



Figure 71. Positional photograph of the Intermec 700C with Belt Clip holster



4.2 PHOTOGRAPHS OF EQUIPMENT UNDER TEST (EUT)

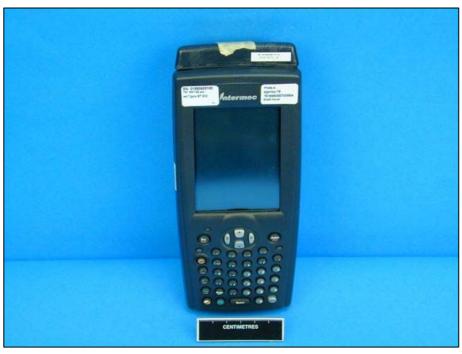


Figure 72: Front View of the Intermec 700C



Figure 73: Rear View of the Intermec 700C



4.2 PHOTOGRAPHS OF EQUIPMENT UNDER TEST (EUT) - Continued



Figure 74: Rear (Internal) View of the Intermec 700C



Figure 75: Front View of the Intermec 700C Holster #1



4.2 PHOTOGRAPHS OF EQUIPMENT UNDER TEST (EUT) - Continued



Figure 76: Front View of the Intermec 700C Holster #2



Figure 77: Front View of the Intermec 700C Belt Clip



SECTION 5

ACCREDITATION, DISCLAIMERS AND COPYRIGHT

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5.1 ACCREDITATION, DISCLAIMERS AND COPYRIGHT

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ANNEX A

PROBE 170 (TYPE IXP-050) CALIBRATION INFORMATION





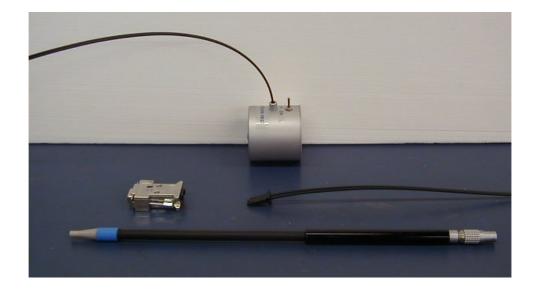
IMMERSIBLE SAR PROBE

CALIBRATION REPORT

Part Number: IXP - 050

S/N 0170

January 2006



IndexSAR Limited Oakfield House Cudworth Lane Newdigate Surrey RH5 5BG Tel: +44 (0) 1306 632 870 Fax: +44 (0) 1306 631 834 e-mail: <u>enquiries@indexsar.com</u>



INTRODUCTION

This Report presents measured calibration data for a particular IndexSAR SAR probe (S/N 0170) and describes the procedures used for characterisation and calibration.

IndexSAR probes are characterised using procedures that, where applicable, follow the recommendations of CENELEC [1] and IEEE [2] standards. The procedures incorporate techniques for probe linearisation, isotropy assessment and determination of liquid factors (conversion factors). Calibrations are determined by comparing probe readings with analytical computations in canonical test geometries (waveguides) using normalised power inputs.

Each step of the calibration procedure and the equipment used is described in the sections below.

CALIBRATION PROCEDURE

1. <u>Objectives</u>

The calibration process comprises three stages

1) Determination of the channel sensitivity factors which optimise the probe's overall rotational isotropy in 1800MHz brain fluid

2) At each frequency of interest, application of these channel sensitivity factors to model the exponential decay of SAR in a waveguide fluid cell, and hence derive the liquid conversion factors at that frequency

3) Determination of the effective tip radius and angular offset of the X channel which together optimise the probe's spherical isotropy in 900MHz brain fluid

2. <u>Probe Output</u>

The probe channel output signals are linearised in the manner set out in Refs [1] and [2]. The following equation is utilized for each channel:

$$U_{lin} = U_{o/p} + U_{o/p}^{2} / DCP$$
 (1)

where U_{lin} is the linearised signal, $U_{o/p}$ is the raw output signal in voltage units and DCP is the diode compression potential in similar voltage units.

DCP is determined from fitting equation (1) to measurements of U_{iin} versus source feed power over the full dynamic range of the probe. The DCP is a characteristic of the Schottky diodes used as the sensors. For the IXP-050 probes with CW signals the DCP values are typically 0.10V (or 20 in the voltage units used by IndexSAR software, which are V*200).

In turn, measurements of E-field are determined using the following equation (where output voltages are also in units of V*200):

$$E_{liq}^{2} (V/m) = U_{linx} * Air Factor_{x} * Liq Factor_{x} + U_{liny} * Air Factor_{y} * Liq Factor_{y} + U_{linz} * Air Factor_{z} * Liq Factor_{z}$$
(3)

Here, "Air Factor" represents each channel's sensitivity, while "Liq Factor" represents the enhancement in signal level when the probe is immersed in tissue-simulant liquids at each frequency of interest.



CALIBRATION PROCEDURE - Continued

3. <u>Selecting Channel Sensitivity Factors To Optimise Isotropic Response</u>

After manufacture, the first stage of the calibration process is to balance the three channels' Air Factor values, thereby optimising the probe's overall axial response ("rotational isotropy").

To do this, an 1800MHz waveguide containing head-fluid simulant is selected. Like all waveguides used during probe calibration, this particular waveguide contains two distinct sections: an air-filled launcher section, and a liquid cell section, separated by a dielectric matching window designed to minimise reflections at the air-liquid interface.

The waveguide stands in an upright position and the liquid cell section is filled with 1800MHz brain fluid to within 10 mm of the open end. The depth of liquid ensures there is negligible radiation from the waveguide open top and that the probe calibration is not influenced by reflections from nearby objects.

During the measurement, a TE_{01} mode is launched into the waveguide by means of an N-type-towaveguide adapter. The probe is then lowered vertically into the liquid until the tip is exactly 10mm above the centre of the dielectric window. This particular separation ensures that the probe is operating in a part of the waveguide where boundary corrections are not necessary.

Care must also be taken that the probe tip is centred while rotating.

The exact power applied to the input of the waveguide during this stage of the probe calibration is immaterial since only relative values are of interest while the probe rotates. However, the power must be sufficiently above the noise floor and free from drift.

The dedicated IndexSAR calibration software rotates the probe in 10 degree steps about its axis, and at each position, an IndexSAR 'Fast' amplifier samples the probe channels 500 times per second for 0.4 s. The raw $U_{o/p}$ data from each sample are packed into 10 bytes and transmitted back to the PC controller via an optical cable. U_{linx} , U_{liny} and U_{linz} are derived from the raw $U_{o/p}$ values and written to an Excel template.

Once data have been collected from a full probe rotation, the Air Factors are adjusted using a special Excel Solver routine to equalise the output from each channel and hence minimise the rotational isotropy. This automated approach to optimisation removes the effect of human bias.

Figure 5 represents the output from each diode sensor as a function of probe rotation angle. The directionality of the orthogonally-arranged sensors can be checked by analysing the data using dedicated IndexSAR software, which displays the data in 3D format, a representative image of which is shown in Figure 3. The left-hand side of this diagram shows the individual channel outputs after linearisation (see above). The program uses these data to balance the channel outputs and then applies an optimisation process, which makes fine adjustments to the channel factors for optimum isotropic response.



CALIBRATION PROCEDURE - Continued

4. Determination Of Conversion ("Liquid") Factors At Each Frequency Of Interest

A lookup table of conversion factors for a probe allows a SAR value to be derived at the measured frequencies, and for either brain or body fluid-simulant.

The method by which the conversion factors are assessed is based on the comparison between measured and analytical rates of decay of SAR with height above a dielectric window. This way, not only can the conversion factors for that frequency/fluid combination be determined, but an allowance can also be made for the scale and range of boundary layer effects.

The theoretical relationship between the SAR at the cross-sectional centre of the lossy waveguide as a function of the longitudinal distance (z) from the dielectric separator is given by Equation 4:

$$SAR(z) = \frac{4(P_f - P_b)}{\rho ab\delta} e^{-2z/\delta}$$
(4)

Here, the density ρ is conventionally assumed to be 1000 kg/m³, *ab* is the cross-sectional area of the waveguide, and P_f and P_b are the forward and reflected power inside the lossless section of the waveguide, respectively. The penetration depth δ (which is the reciprocal of the waveguide-mode attenuation coefficient) is a property of the lossy liquid and is given by Equation (5).

$$\delta = \left[\operatorname{Re}\left\{ \sqrt{\left(\pi / a\right)^{2} + j\omega\mu_{o}\left(\sigma + j\omega\varepsilon_{o}\varepsilon_{r}\right)} \right\} \right]^{-1}$$
(5)

where σ is the conductivity of the tissue-simulant liquid in S/m, ε_r is its relative permittivity, and ω is the radial frequency (rad/s). Values for σ and ε_r are obtained prior to each waveguide test using an IndexSAR DiLine measurement kit, which uses the TEM method as recommended in [2]. σ and ε_r are both temperature- and fluid-dependent, so are best measured using a sample of the tissue-simulant fluid immediately prior to the actual calibration.

Wherever possible, all DiLine and calibration measurements should be made in the open laboratory at 22 \pm 2.0°C; if this is not possible, the values of σ and ε_r should reflect the actual temperature. Values employed for calibration are listed in the tables below.

By ensuring the liquid height in the waveguide is at least three penetration depths, reflections at the upper surface of the liquid are negligible. The power absorbed in the liquid is therefore determined solely from the waveguide forward and reflected power.

Different waveguides are used for 835/900MHz, 1800/1900MHz, 2450MHz and 5200/5800MHz measurements. Table A.1 of [1] can be used for designing calibration waveguides with a return loss greater than 20 dB at the most important frequencies used for personal wireless communications, and better than 15dB for frequencies



CALIBRATION PROCEDURE - Continued

4. <u>Determination Of Conversion ("Liquid") Factors At Each Frequency Of Interest</u> -Continued

greater than 5GHz. Values for the penetration depth for these specific fixtures and tissue-simulating mixtures are also listed in Table A.1.

According to [1], this calibration technique provides excellent accuracy, with standard uncertainty of less than 3.6% depending on the frequency and medium. The calibration itself is reduced to power measurements traceable to a standard calibration procedure. The practical limitation to the frequency band of 800 to 5800 MHz because of the waveguide size is not severe in the context of compliance testing.

During calibration, the probe is lowered carefully until it is just touching the cross-sectional centre of the dielectric window. 200 samples are then taken and written to an Excel template file before moving the probe vertically upwards. This cycle is repeated 50 times. The vertical separation between readings is determined from practical considerations of the expected SAR decay rate, and range from 1mm steps at low frequency, through 0.5mm at 2450MHz, down to 0.2mm at 5GHz.

Once the data collection is complete, a Solver routine is run which optimises the measuredtheoretical fit by varying the conversion factor, and the boundary correction size and range.

5. Measurement of Spherical Isotropy

The setup for measuring the probe's spherical isotropy is shown in Figure 2.

A box phantom containing 900MHz head fluid is irradiated by a vertically-polarised, tuned dipole, mounted to the side of the phantom on the robot's seventh axis. During calibration, the spherical response is generated by rotating the probe about its axis in 20 degree steps and changing the dipole polarisation in 10 degree steps.

By using the VPM technique discussed below, an allowance can also be made for the effect of Efield gradient across the probe's spatial extent. This permits values for the probe's effective tip radius and X-channel angular offset to be modelled until the overall spherical isotropy figure is optimised.

The dipole is connected to a signal generator and amplifier via a directional coupler and power meter. As with the determination of rotational isotropy, the absolute power level is not important as long as it is stable.

The probe is positioned within the fluid so that its sensors are at the same vertical height as the centre of the source dipole. The line joining probe to dipole should be perpendicular to the phantom wall, while the horizontal separation between the two should be small enough for VPM corrections to be applicable, without encroaching near the boundary layer of the phantom wall. VPM corrections require a knowledge of the fluid skin depth. This is measured during the calibration by recording the E-field strength while systematically moving the probe away from the dipole in 2mm steps over a 20mm range.

VPM (Virtual Probe Miniaturisation)

SAR probes with 3 diode-sensors in an orthogonal arrangement are designed to display an isotropic response when exposed to a uniform field. However, the probes are ordinarily used for measurements in non-uniform fields and isotropy is not



CALIBRATION PROCEDURE – Continued

5. <u>Measurement of Spherical Isotropy</u> - Continued

assured when the field gradients are significant compared to the dimensions of the tip containing the three orthogonally-arranged dipole sensors.

It becomes increasingly important to assess the effects of field gradients on SAR probe readings when higher frequencies are being used. For IndexSAR IXP-050 probes, which are of 5mm tip diameter, field gradient effects are minor at GSM frequencies, but are major above 5GHz. Smaller probes are less affected by field gradients and so probes, which are significantly less than 5mm diameter, would be better for applications above 5GHz.

The IndexSAR report IXS0223 describes theoretical and experimental studies to evaluate the issues associated with the use of probes at arbitrary angles to surfaces and field directions. Based upon these studies, the procedures and uncertainty analyses referred to in P1528 are addressed for the full range of probe presentation angles.

In addition, generalized procedures for correcting for the finite size of immersible SAR probes are developed. Use of these procedures enables application of schemes for virtual probe miniaturization (VPM) – allowing probes of a specific size to be used where physically-smaller probes would otherwise be required.

Given the typical dimensions of 3-channel SAR probes presently available, use of the VPM technique extends the satisfactory measurement range to higher frequencies.

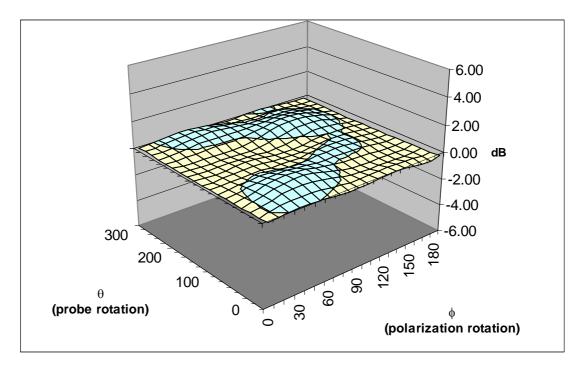


CALIBRATION FACTORS MEASURED FOR PROBE S/N 0170

The probe was calibrated at 835, 900, 1800, 1900, 2450, 5200 and 5800 MHz in liquid samples representing both brain liquid and body fluid at these frequencies. The calibration was for CW signals only, and the axis of the probe was parallel to the direction of propagation of the incident field i.e. end-on to the incident radiation. The axial isotropy of the probe was measured by rotating the probe about its axis in 10 degree steps through 360 degrees in this orientation.

The reference point for the calibration is in the centre of the probe's cross-section at a distance of 2.7 mm from the probe tip in the direction of the probe amplifier. A value of 2.7 mm should be used for the tip to sensor offset distance in the software. The distance of 2.7mm for assembled probes has been confirmed by taking X-ray images of the probe tips (see Figure 8).

It is important that the diode compression point and air factors used in the software are the same as those quoted in the results tables, as these are used to convert the diode output voltages to a SAR value.



Surface Isotropy diagram of IXP-050 Probe S/N 0170 at 900MHz after VPM (rotational isotropy at side +/-0.13dB, spherical isotropy +/-0.24dB)

Probe tip radius	1.25
X Ch. Angle to red dot	0.2



	Head			Body
Frequency	Bdy. Corrn. – f(0)	Bdy. Corrn. – d(mm)	Bdy. Corrn. – f(0)	Bdy. Corrn. – d(mm)
450	-	-	-	-
835	0.51	3.0	0.67	2.9
900	0.54	3.0	0.72	3.0
1800	1.00	1.2	0.71	1.5
1900	1.00	1.2	0.61	1.7
2000	1.00	1.2	0.58	1.7
2450	0.88	1.3	0.65	1.8

CALIBRATION FACTORS MEASURED FOR PROBE S/N 0170 - Continued

SUMMARY OF CALIBRATION FACTORS FOR PROBE IXP-050 S/N 0170

Spherical isotropy measured at 900MHz	0.24	(+/-) dB
---------------------------------------	------	-------------

	Х	Y	Z	
Air Factor s	433	367	399	(V*200)
CW DCPs	20	20	20	(V*200)

Freq	Axi	al Isotropy	S	AR ConvF	
(MHz		(+/- dB)		(liq/air)	Notes
)	Head	Body	Head	Body	
450	-	-	0.297	0.295	
835	-	-	0.260	0.276	1,2
900	-	-	0.264	0.287	1,2
1800	0.13	-	0.281	0.307	1,2
1900	-	-	0.286	0.324	1,2
2000	-	-	0.290	0.326	1,2
2450	-	-	0.335	0.384	1,2

Notes	
1)	Calibrations done at 22°C +/-2°C
2)	Waveguide calibration



PROBE SPECIFICATIONS

IndexSAR probe 0170, along with its calibration, is compared with CENELEC and IEEE standards recommendations (Refs [1] and [2]) in the Tables below. A listing of relevant specifications is contained in the tables below:

Dimensions	S/N 0170	CENELEC [1]	IEEE [2]
Overall length (mm)	350		
Tip length (mm)	10		
Body diameter (mm)	12		
Tip diameter (mm)	5.2	8	8
Distance from probe tip to dipole centers (mm)	2.7		

Dunomio rongo	S/N 0170		
Dynamic range	5/N 0170	CENELEC [1]	IEEE [2]
Minimum (W/kg)	0.01	<0.02	0.01
Maximum (W/kg)	>100	>100	100
N.B. only measured to > 100			
W/kg on representative probes			

Isotropy (measured at 900MHz)	S/N 0170	CENELEC [1]	IEEE [2]
Axial rotation with probe	0.13 Max	0.5	0.25
normal to source (+/- dB)	(See table above)		
Spherical isotropy covering all	0.24	1.0	0.50
orientations to source (+/- dB)			

Construction	Each probe contains three orthogonal dipole sensors arranged on a triangular prism core, protected against static charges by built-in shielding, and covered at the tip by PEEK cylindrical enclosure material. No adhesives are used in the immersed section. Outer case materials are PEEK and heat- shrink sleeving.
Chemical resistance	Tested to be resistant to glycol and alcohol containing simulant liquids but probes should be removed, cleaned and dried when not in use.

REFERENCES

[1] CENELEC, EN 50361, July 2001. Basic Standard for the measurement of specific absorption rate related to human exposure to electromagnetic fields from mobile phones.

[2] IEEE 1528, Recommended practice for determining the spatial-peak specific absorption rate (SAR) in the human body due to wireless communications devices: Experimental techniques.



FIGURES



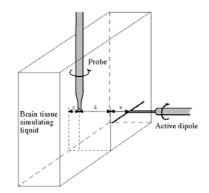


Figure 1. Spherical isotropy jig showing probe, dipole and box filled with simulated brain liquid (see Ref [2], Section A.5.2.1)

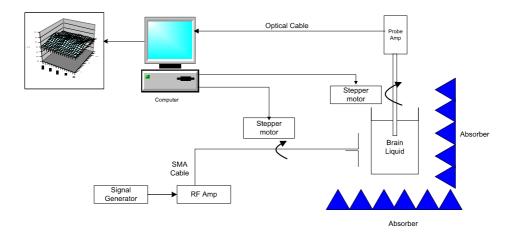


Figure 2. Schematic diagram of the test geometry used for isotropy determination



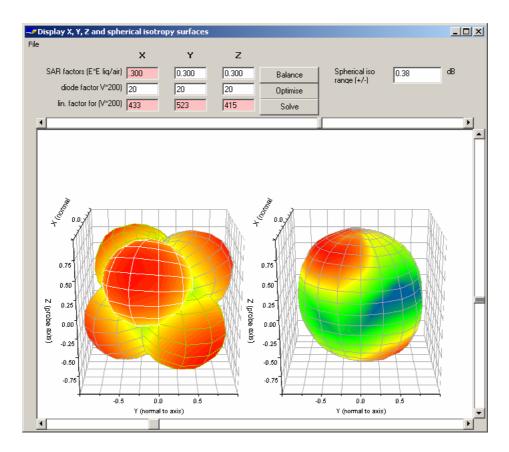


Figure 3. Graphical representation of a probe's response to fields applied from each direction. The diagram on the left shows the individual response characteristics of each of the three channels and the diagram on the right shows the resulting probe sensitivity in each direction. The colour range in the figure images the lowest values as blue and the maximum values as red. For the probe S/N 0170, this range is (+/-) 0.24 dB.

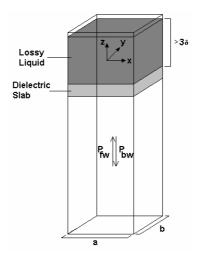


Figure 4. Geometry used for waveguide calibration (after Ref [2]. Section A.3.2.2)



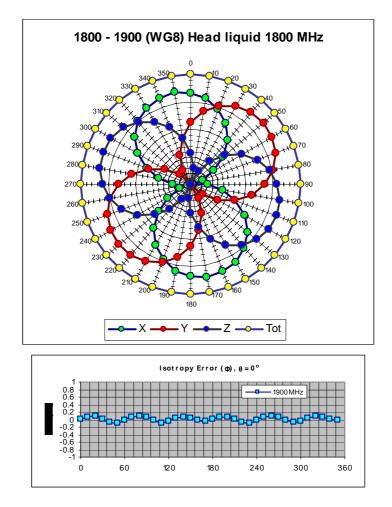
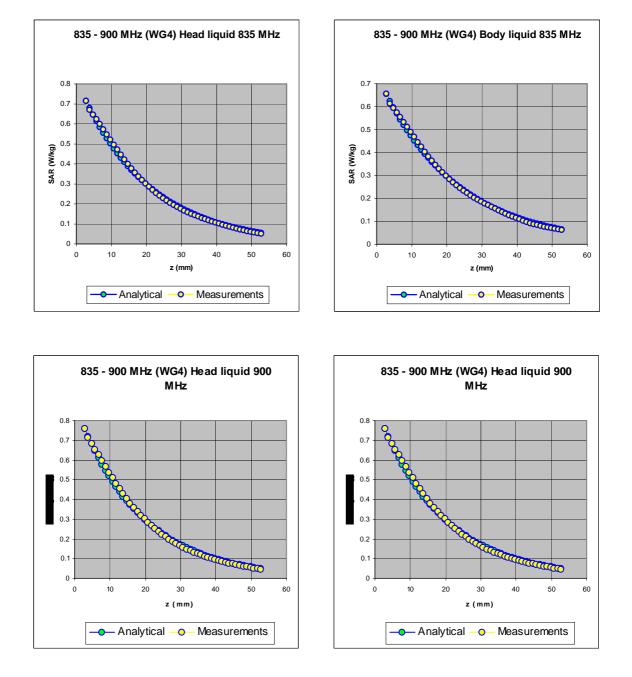


Figure 5. The rotational isotropy of probe S/N 0170 obtained by rotating the probe in a liquid-filled waveguide at 1800 MHz.

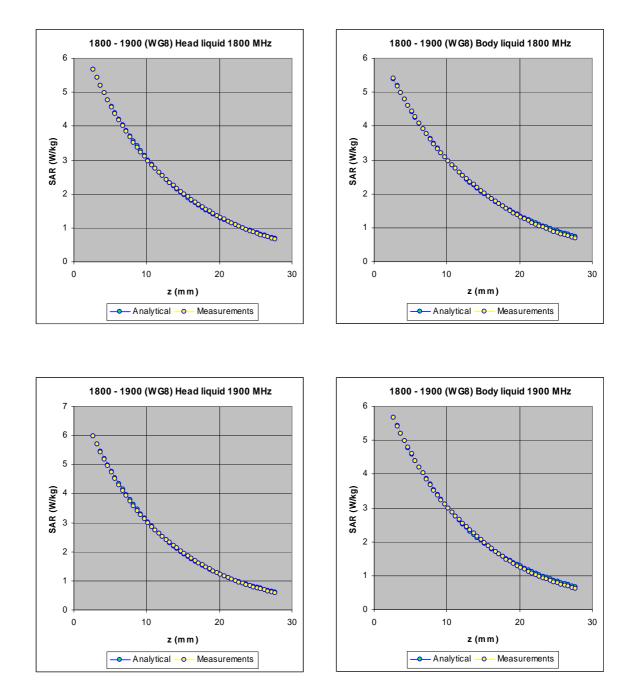




SAR DECAY FUNCTION – Analytical and Measurements

Figure 6a. The measured SAR decay function along the centreline of the WG4 waveguide with conversion factors adjusted to fit to the theoretical function for the particular dimension, frequency, power and liquid properties employed.

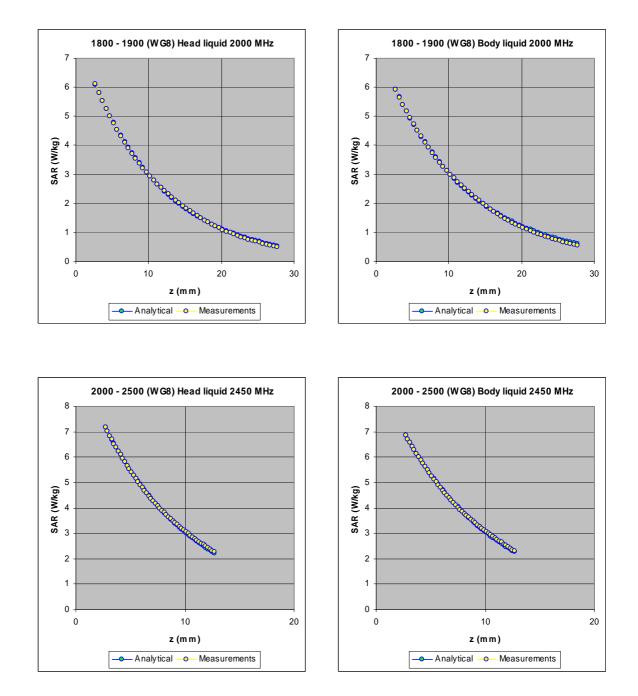




SAR DECAY FUNCTION - Analytical and Measurements - Continued

Figure 6b The measured SAR decay function along the centreline of the WG4 waveguide with conversion factors adjusted to fit to the theoretical function for the particular dimension, frequency, power and liquid properties employed.





SAR DECAY FUNCTION – Analytical and Measurements - Continued

Figure 6c The measured SAR decay function along the centreline of the R22 waveguide with conversion factors adjusted to fit to the theoretical function for the particular dimension, frequency, power and liquid properties employed.



SAR DECAY FUNCTION - Analytical And Measurements - Continued

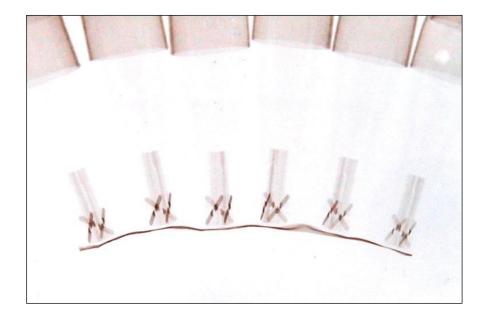


Figure 8: X-ray positive image of 5mm probes

TABLE INDICATING THE DIELECTRIC PARAMETERS OF THE LIQUIDS USED FOR CALIBRATIONS AT EACH FREQUENCY

Liquid used	Relative permittivity (measured)	Conductivity (S/m) (measured)
835 MHz BRAIN	41.38	0.90
835 MHz BODY	58.97	0.94
900 MHz BRAIN	40.59	0.96
900 MHz BODY	58.45	1.01
1800 MHz BRAIN	39.21	1.44
1800 MHz BODY	54.76	1.59
1900 MHz BRAIN	38.73	1.54
1900 MHz BODY	54.42	1.70
2000 MHz BRAIN	38.28	1.64
2000 MHz BODY	54.09	1.81
2450 MHz BRAIN	38.86	1.98
2450 MHz BODY	52.48	2.16



PROBE 190 (TYPE IXP-050) CALIBRATION INFORMATION



	NATIONAL PHYSICAL LABORATORY Teddington Middlesex UK TW11 0LW Switchboard 020 8977 3222
	Certificate of Calibration
	SAR PROBE IndexSAR Model: IXP-050 Serial number: 0190
	REPLACEMENT CERTIFICATE FOR: E05070339
bar t	FOR:. TUV Product Services Ltd / BABT Octagon House Concorde Way Segensworth North Fareham Hampshire PO15 5RL
	DESCRIPTION: An IndexSAR isotropic electric field probe for determining specific absorption rates (SAR) in dielectric liquids. The probe has three orthogonal sensors, and the output voltage of the sensors is converted to an optical signal by a meter unit containing an analogue to digital (AD) converter. Probe readings are obtained using software via the RS232 port. The probe was calibrated with IndexSAR amplifier model IXA-010 S/N 036 belonging to NPL.
	IDENTIFICATION: The probe is marked with the manufacturer's serial number 0190.
	MEASUREMENTS COMPLETED ON: 20 – 22 July 2005
	PREVIOUS NPL CERTIFICATE: None
	The reported uncertainty is based on a coverage factor $k = 2$, providing a level of confidence of approximately 95%
	Reference : E05070339R Page 1 of 4
	Date of Issue : 22 November 2005Signed : D C Centrel (Authorised Signatory)Checked by : B loaderName : Mr D G Gentlefor Managing Director
NPL-C14-99/11	This certificate provides traceability of measurement to recognised national standards, and to the units of measurement realised at the NPL or other recognised national standards laboratories. This certificate may not be reproduced other than in full, unless permission for the publication of an approved extract has been obtained in writing from the Managing Director. It does not of itself impute to the subject of calibration any attributes beyond those shown by the data contained herein.



NATIONAL PHYSICAL LABORATORY

Continuation Sheet

MEASUREMENT PROCEDURE

The calibration method is based on establishing a calculable specific absorption rate (SAR) using a matched waveguide cell [1]. The cell has a feed-section and a liquid-filled section separated by a matching window that is designed to minimise reflections at the interface. A TE_{01} mode is launched into the waveguide by means of a N-type-to-waveguide adapter. The power delivered to the liquid is calculated from the forward power and reflection coefficient measured at the input to the cell. At the centre of the cross-section of the waveguide cell, the volume specific absorption rate (*SAR^V*) in the liquid as a function of distance from the window is given by

$$SAR^{V} = \frac{4(P_{w})}{ab\delta}e^{-2Z/\delta}$$
(1)

where

a = the larger cross-sectional dimension of the waveguide.

b = the smaller cross-sectional dimension of the waveguide.

 δ = the skin depth for the liquid in the waveguide.

Z = the distance of the probe's sensors from the liquid to matching window boundary.

 P_w = the power delivered to the liquid.

Liquids having the properties specified by CENELEC and IEEE Standards [2,3] were used for the calibration. The value of δ for the liquid was obtained by measuring the electric field (*E*) at a number of distances from the matching window. The calibration was for continuous wave (CW) signals, and the axis of the probe was parallel to the direction of propagation of the incident field i.e. end-on to the incident radiation. The probe was rotated about its axis in 15degree steps, and the ratio of the calibration factors for the three probe sensors X, Y, & Z were optimized to give the best axial isotropy.

The probe was calibrated with the linearisation and air-correction factors enabled. Comparing the measured values of E^2 in the liquid to those calculated for the waveguide cell allows the ratio, *ConvF*, of sensitivity for $(E^2_{LIQUID}) / (E^2_{AIR})$ to be determined, as required by the probe software.

ENVIRONMENT

Measurements were made in a temperature-controlled laboratory at 22 ± 1 °C. The temperature of the liquid used was measured at the beginning and end of each measurement.

Reference : E05070339R

Page 2 of 4

Date of Issue : 22 November 2005 Checked by : Bld -

NPL-A01-94/1



	NATIONAL PHYSICAL LABORATORY Continuation Sheet	
	UNCERTAINTIES .	
	The estimated uncertainty in calibration for SAR (W kg ⁻¹) is \pm 10 %. The reported uncertainty is based on a standard uncertainty multiplied by a coverage factor $k = 2$, providing a level of confidence of approximately 95%.	
	This uncertainty is valid when the probe is used in a liquid with the same dielectric properties as those used for the calibration. No estimate is made for the long-term stability of the device calibrated or of the fluids used in the calibration.	
	When using the probe for SAR testing, additional uncertainties should be added to account for the spherical isotropy of the probe, proximity effects, linearity, and response to pulsed fields. There will be additional uncertainty if the probe is used in liquids having significantly different electrical properties to those used for the calibration. The electrical properties of the liquids will be related to temperature.	
	RESULTS	
	Table 1 gives the results for calibration in liquid.	
	These calibration factors are only correct when the values for sensitivity in free-space, diode compression and sensor offset from the tip of the probe, as set in the probe software, are the same as those given in Table.	
	REFERENCES:	
	 Pokovic et al 1997, Pokovic, KT, T.Schmid and N.Kuster, "Robust set-up for Precise Calibration of E-field probes in Tissue Simulating Liquids at Mobile Phone Frequencies", Proceedings ICECOM 1997, pp 120 – 124, Dubrovnik, Croatia Oct 12-17, 1997. 	
	[2] British Standard BS EN 503361:2001. "Basic standard for the measurement of specific absorption rate related to human exposure to electromagnetic fields from mobile phones $(300 \text{ MHz} - 3 \text{ GHz})$ ".	
	[3] IEEE Standard 1528-2003 "Recommended Practice for Determining the Peak Spatial- Averaged Specific Absorption Rate (SAR) in the Human Head from Wireless Communications Devices: Measurement Techniques".	
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			ensitivity AR prob	ole 1 in Liquids e: IXP-050 0190					
Probe settings for calibration									
Sensitivity	Diode Compression ⁽¹⁾			Sens	Sensor offset from tip of probe ⁽¹⁾				
Lin Y = 4250	(V/m) ² /(V*200) (V/m) ² /(V*200) (V/m) ² /(V*200)	DCP _X = 20 (V*200) DCP _Y = 20 (V*200) DCP _z = 20 (V*200)			2.7 mm				
Sensitivity in Liquid.									
Calibration frequency	12420200000000 1000000 1000000 1000000		bration Factors for E^2_{Liquid} / E^2_{Air}		Axial Isotrop				
(MHz)	Identifier	ε' ⁽³⁾	σ ⁽³⁾ (Sm ⁻¹)	ConvF _X	ConvF _Y	ConvFz	(dB)		
900	TWS900B-1	56.5	1.00	0.35	0.32	0.36	±0.01		
900	900 Cenelec	40.9	0.94	0.34	0.30	0.33	±0.02		
1800	TWS1800B-2	53.9	1.54	0.44	0.37	0.43	±0.03		
1800	TWS1800H-1	40.6	1.37	0.40	0.34	0.39	±0.02		
1900	NPL1950B-1	39.9	1.45	0.40	0.34	0.40	±0.03		
2450	TWS2450B-2	53.6	2.02	0.49	0.41	0.48	±0.03		
2450	TWS2450H-1	38.7	1.79	0.44	0.37	0.43	±0.03		

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